

VIBE PROJECT

Virtual Biomedical and STEM/STEAM Education

2021-1-HU01-KA220-HED-000032251



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VIBE
PROJECT

PATTERN RECOGNITION IN BIOMEDICAL ENGINEERING

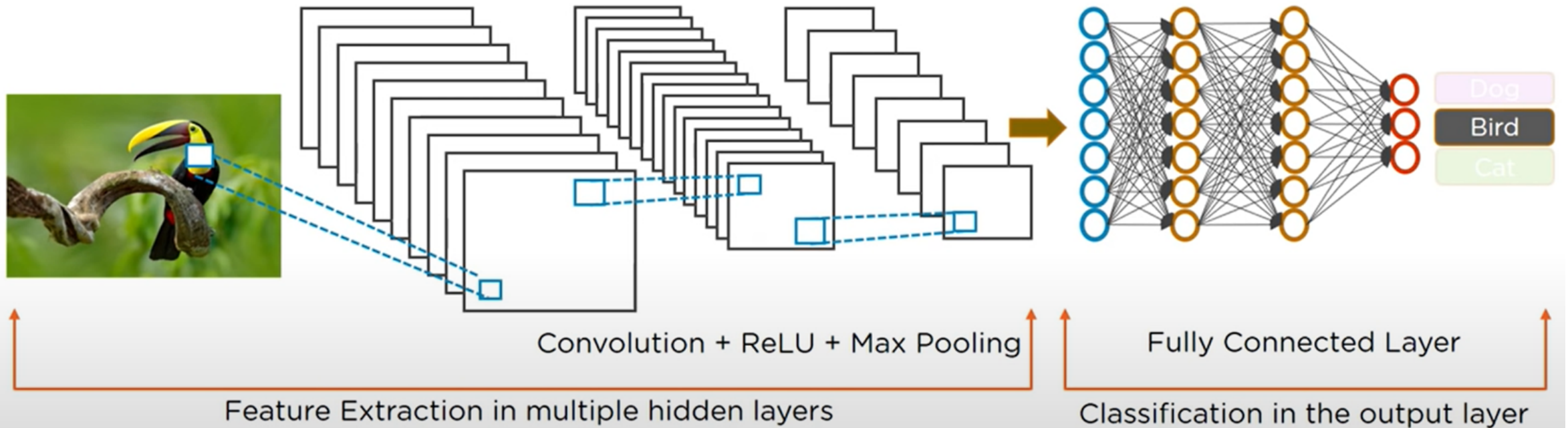
ADVANCED TECHNIQUES IN PATTERN RECOGNITION
- FROM FEATURES TO RECOGNITION SYSTEMS



The total process of object recognition using CNNs



Lets see the entire process how CNN recognizes a bird

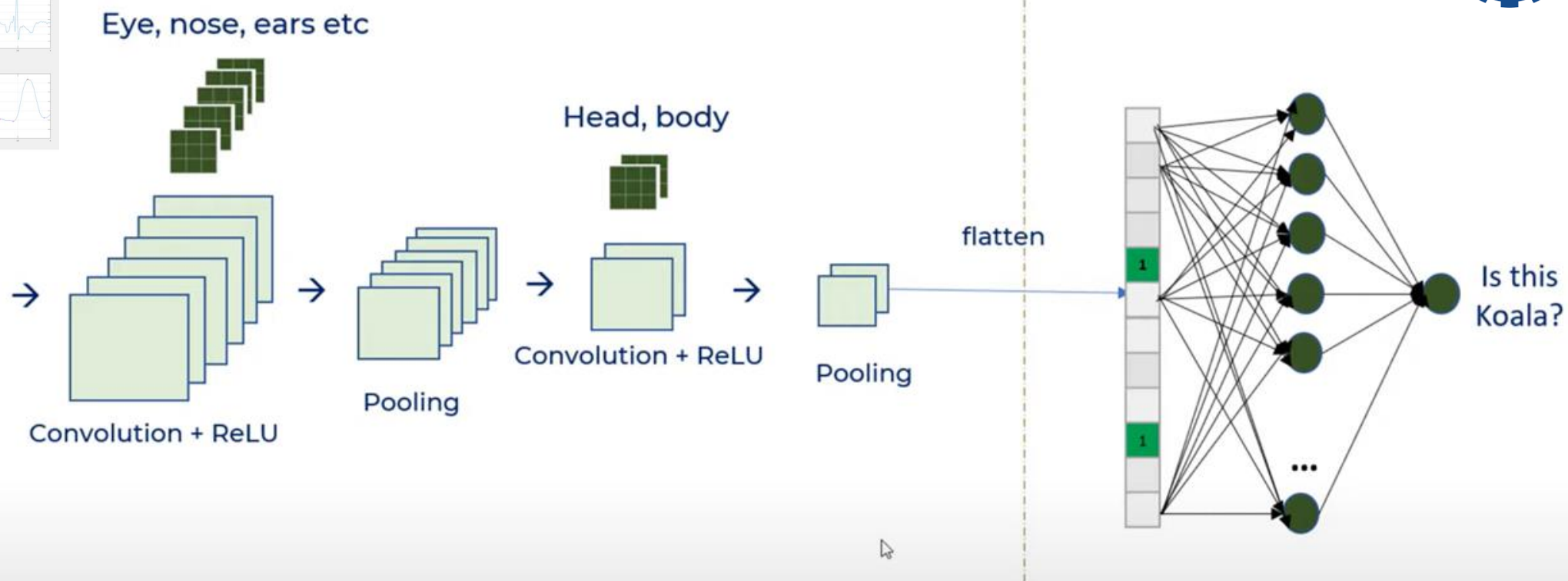
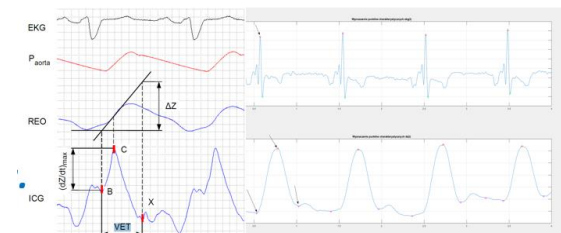


Source: <https://medium.com/ml-cheat-sheet/convolutional-neural-networks-186870efbf71>





Total process of object recognition using CNNs



Source: <https://medium.com/ml-cheat-sheet/convolutional-neural-networks-186870efbf71>

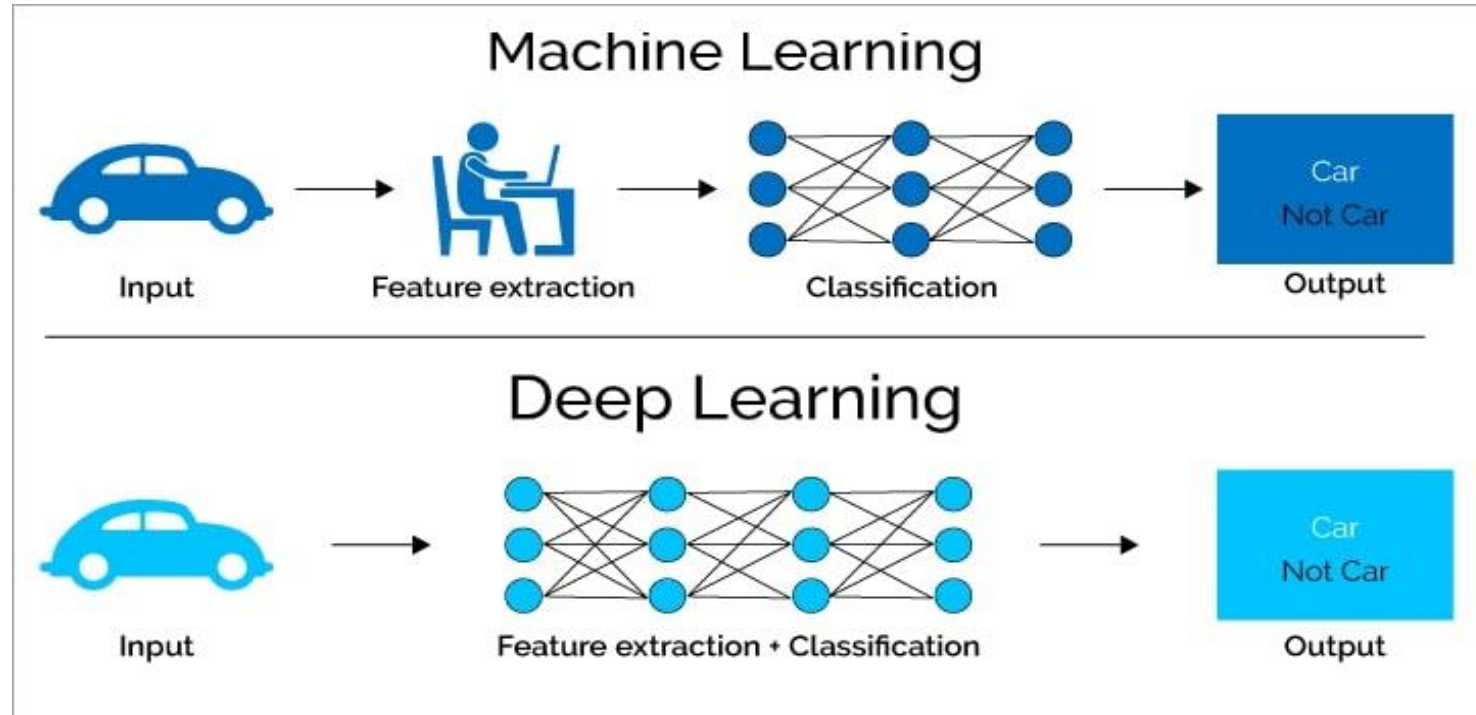


Barn owl or apple? This example indicates how challenging learning from samples is – even for machine learning.

Source: <https://viso.ai/deep-learning/deep-learning-vs-machine-learning/>

@teenybiscuit





Source: <https://levity.ai/blog/difference-machine-learning-deep-learning>

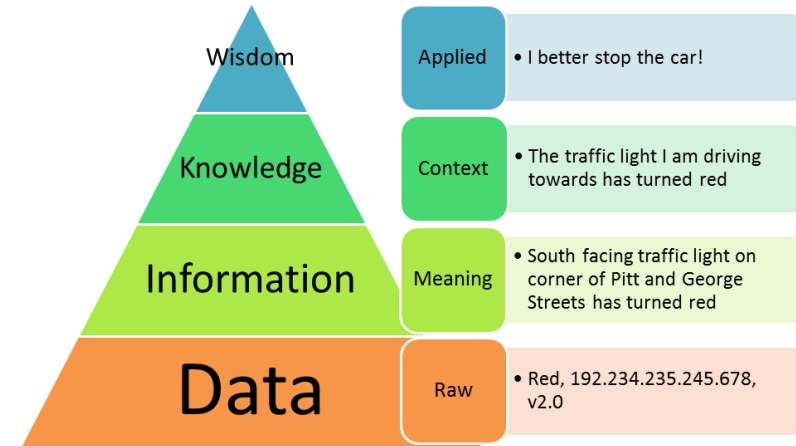
In deep neural networks (DNN), **knowledge is abstractly represented** by weights (numbers) in the context of the problem being analyzed.





Agenda

- Short intro (*back to the past..*): why **digital**? ..signal processing (DSP),
- Our tools from DSP - How we can 'look at' signals in digital form and process them:
 - Time domain methods (→ T_Features)
 - Frequency domain methods (→ F_Features)
 - Time-Frequency domain methods (→ T-F_Features)
- Use cases from the area of modern Biomedical Engineering:
 - Different application examples but a common 'denominator', which are DSP methods

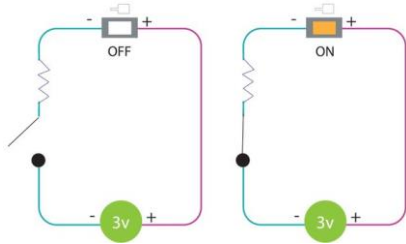


Source: <https://youthgrowth.in/dikw-data-information-knowledge-and-wisdom/>

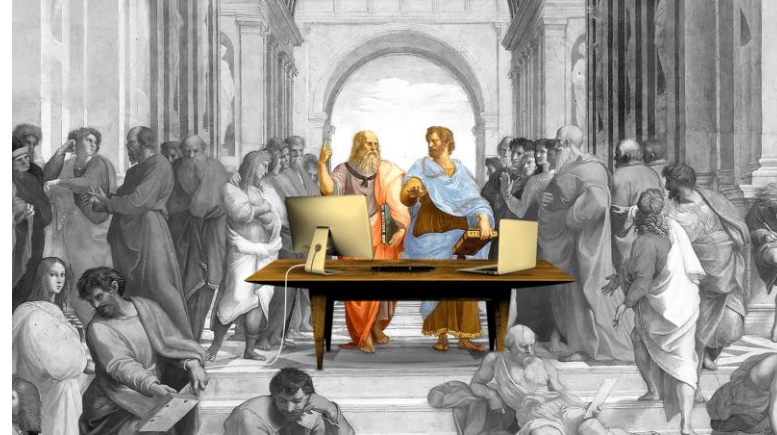
Intro: but why 'digital' processing? ...

Technology :

Only two electrical states to store: 0/1, H/L, T/F (On/Off; H/L, 1/0, +U/GND)

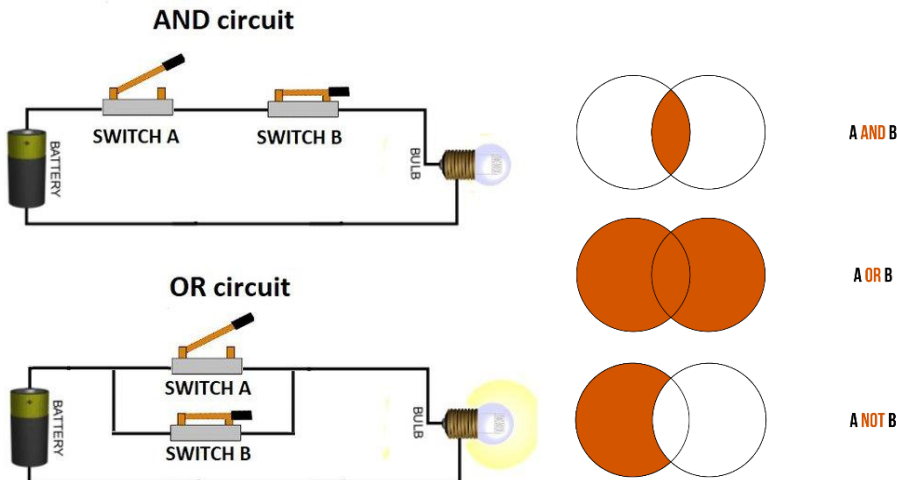
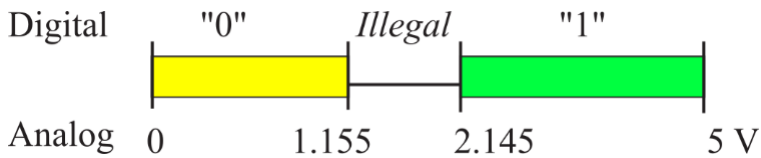
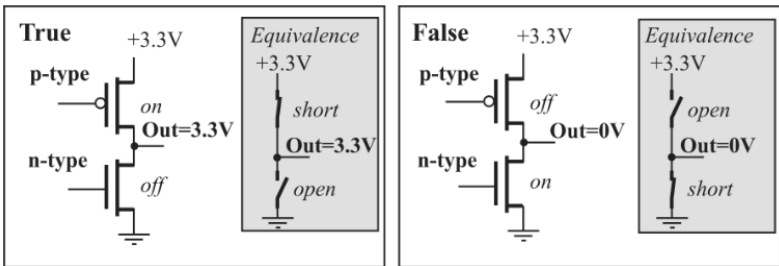


Two level LOGIC development (T/F) – a discipline of science much older than mathematics and goes back to the very beginnings of European science, namely ancient Greece. Even then, it was already performing as a basic tool of philosophical thinking.

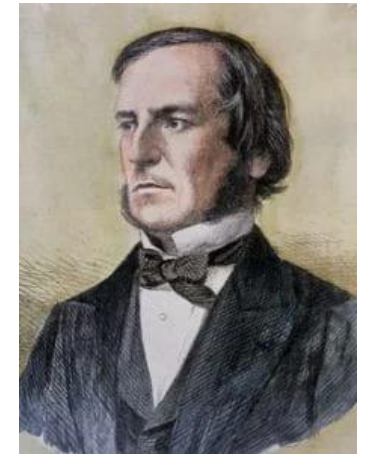


Source: *How Aristotle Created the Computer*

Computers store all information as a sequence of 0 and 1



Boole's Algebra



Source: https://pl.wikipedia.org/wiki/Algebra_Boole%E2%80%99a

Source: Original work by the author.

has been valid and in use since the idea of the first computers in the 1930s, 1940s until today ...

Alan Turing

A genius ahead of the era



- In the 1930s he laid the foundations of theoretical computer science with **binary 0/1 data representation**,
- He defined the term: "computation" ,
- He proposed a computational model called the Turing machine.

What did he have at his disposal at that time ...?

- *A sheet of paper,*
- *A pencil and ...*
- *??*



Source:

https://en.wikipedia.org/wiki/Alan_Turing

*He **created the concept of a computer**, with binary 0/1 data representation, which according to its basic principle still works today (of course, technology has made great progress).*





Alan Turing, 1933-1936,

What can an abstract man count with his own head, a piece of paper, an eraser and a pencil.

a brilliant mathematician, cryptologist ...

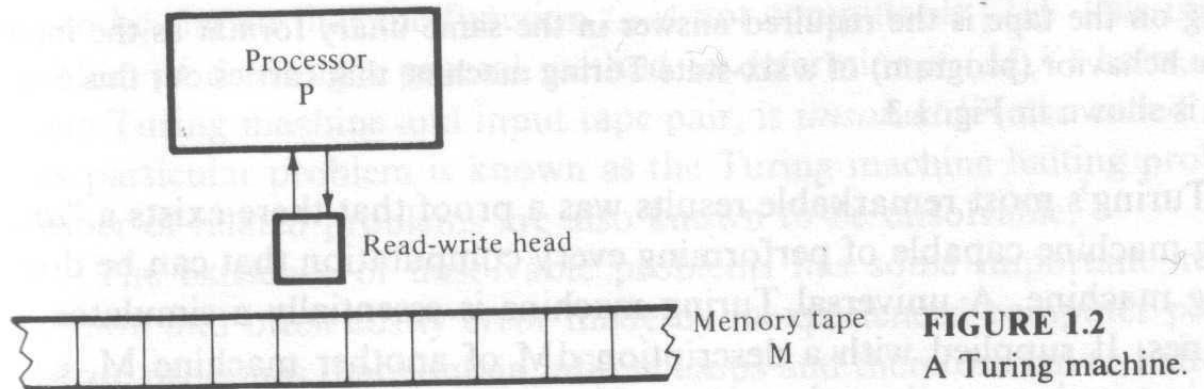
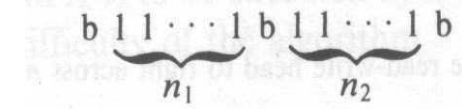


FIGURE 1.2
A Turing machine.

Source:

https://en.wikipedia.org/wiki/Alan_Turing



Instruction		Comments	
s_0	b R s_0		
s_0	1 R s_1	Move read-write head to right across n_1	
s_1	1 R s_1		
s_1	b 1 s_2	Replace blank between n_1 and n_2 by 1	
s_2	1 L s_3	Move read-write head to left	
s_3	1 L s_3		
s_3	b R s_4	End of 1s reached; backspace	
s_4	1 b s_5	Delete leftmost 1	
s_5	b H s_0	$n_1 + n_2$ now on tape	

FIGURE 1.3
A Turing machine program to add two unary numbers.



SMALL-SCALE EXPERIMENTAL MACHINE



19/7/48
 Kilburn Highest Factor Routine (amended)

instr.	C	26	26	27	line	01234	1345
-24 C	-G ₁	-	-	-	1	00011	010
← to 26			-G ₁		2	01011	110
-26 C	G ₁				3	01011	010
← to 27			-G ₁	G ₁	4	11011	110
-23 C	a	T ₂₁	-G ₂	G ₂	5	11101	010
subr 27	a-als				6	1.011	001
test					7	-	011
add 20 to 6					8	00101	100
subr. 26	T ₂₁				9	01011	001
← to 25		T ₂₁			10	10011	110
-25 C					11	10011	010
test					12	-	011
stop	0	0	-G ₂	G ₂	13		111
-26 C	G ₂	T ₂₁	-G ₂	G ₂	14	01011	010
subr. 21	G ₂ !				15	10101	001
← to 27	G ₂ !			G ₂ !	16	11011	110
-27 C	G ₂ !				17	11011	010
← to 26			-G ₂ !		18	01011	110
22 to 6	T ₂₁	-G ₂ !	G ₂ !		19	01101	000

20	-3	10111 etc	23	-a
21	1	10000	24	G ₁
22	4	00100		

or 10100

SSEM (another name for Baby) is the first computer based on the von Neumann technique mentioned earlier. For the first time in history on this computer ran a program stored in its memory (June 21, 1948) this program was created by Tom Kilburn – one of the first Programmers 😊 (his manuscript can be seen in the photo).

The creators, the "geniuses" of computer science wrote the first programs directly in the machine language of the computer: 0110 0101 .

Source:
https://it.wikipedia.org/wiki/Small_Scale_Experimental_Machine

See the brief history of programming languages:
https://www.youtube.com/watch?v=mhpslN-OD_o



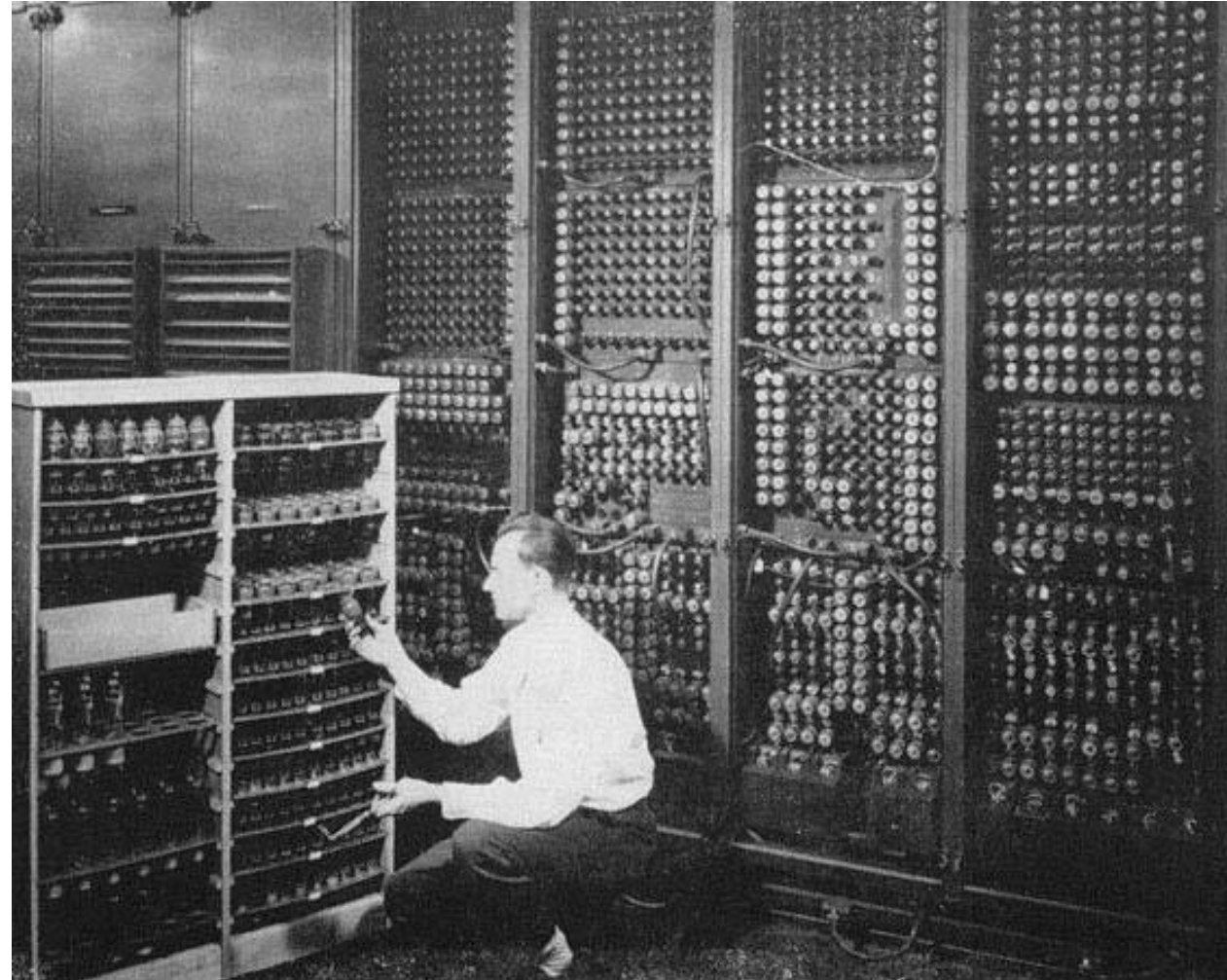
ENIAC 1944

ENIAC 1944 - one of the first computers

(not to be confused with calculators, shown earlier - a computer works according to a program, it is programmed and performs a set of tasks specified by a human)



12 x 6 m
30 tons
70,000 resistors
10 000 capacitors
6,000 switches
18,000 el. lamps
100,000 operations/s



Source: <https://en.wikipedia.org/wiki/ENIAC>

Silicon revolution: semiconductors, TRANSISTORS enable to ,store' 0/1, H/L

Decades of Silicon Valley Innovation*



Tube

1930s - Radio Communications (Litton)

1940s - Defense Systems (Varian)

1950s - Magnetic Storage (IBM)



Transistor

1960s - Semiconductors (Fairchild)

1970s - Personal Computing (Apple)



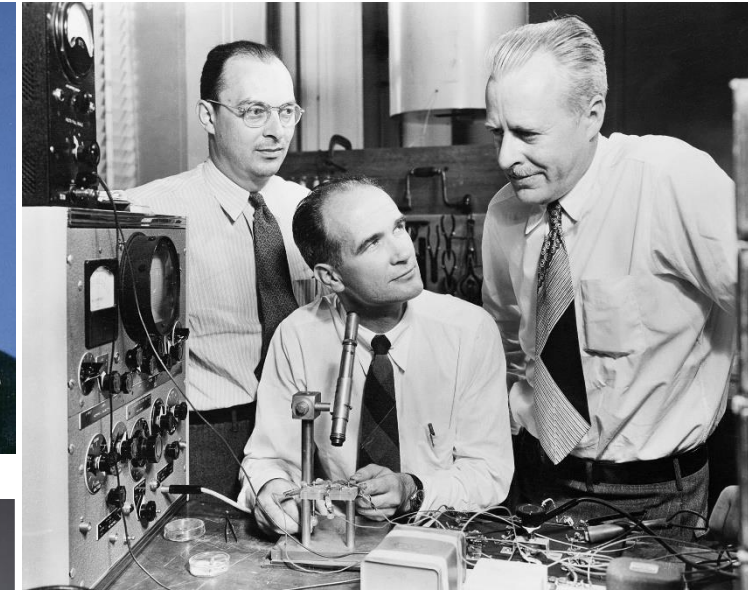
Microchip

1980s - Networks (Xerox)

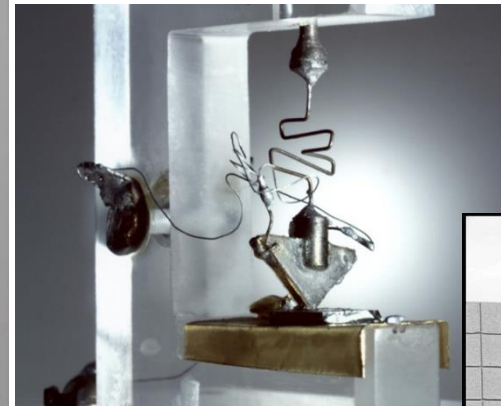
1990s - Internet (Cisco)

2000s - Mobile (Apple)

* in hardware



Source: John Bardeen, William Shockley and Walter Brattain at Bell Labs, 1948



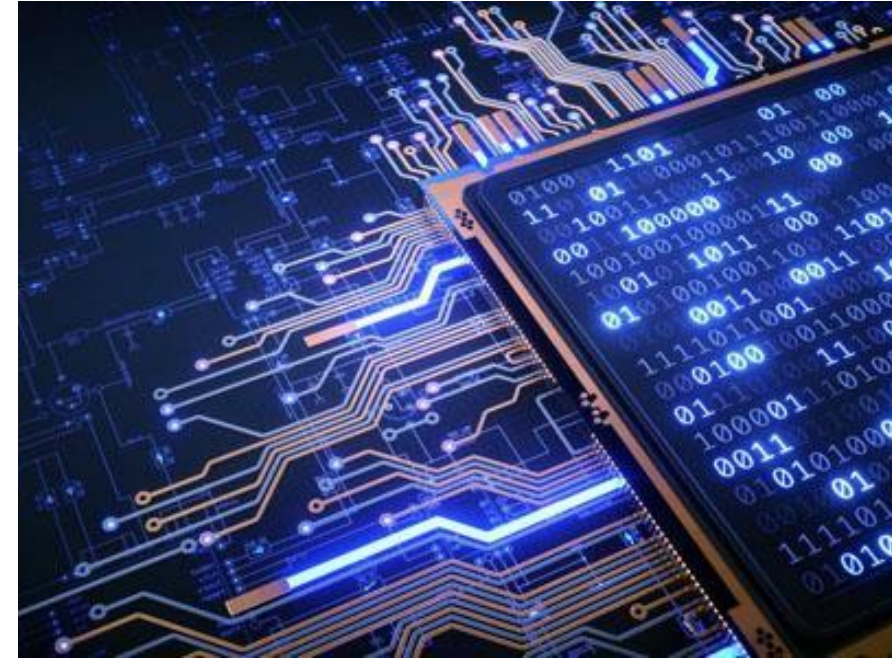
<https://www.pbs.org/wgbh/americanexperience/features/silicon-timeline-silicon/>
<https://computerhistory.org/blog/silicon-valley-a-century-of-entrepreneurial-innovation/>

Source: https://en.wikipedia.org/wiki/History_of_the_transistor

Semiconductor scientists and engineers hold a **secret meeting at San Francisco's Clift Hotel** to discuss forming their own firm, under the leadership of Robert Noyce. The men would come to be known as the "Traitorous Eight."

For a computer, **any information** (data, image, sound, char, graphic, etc.)

is a **NUMBER !!**

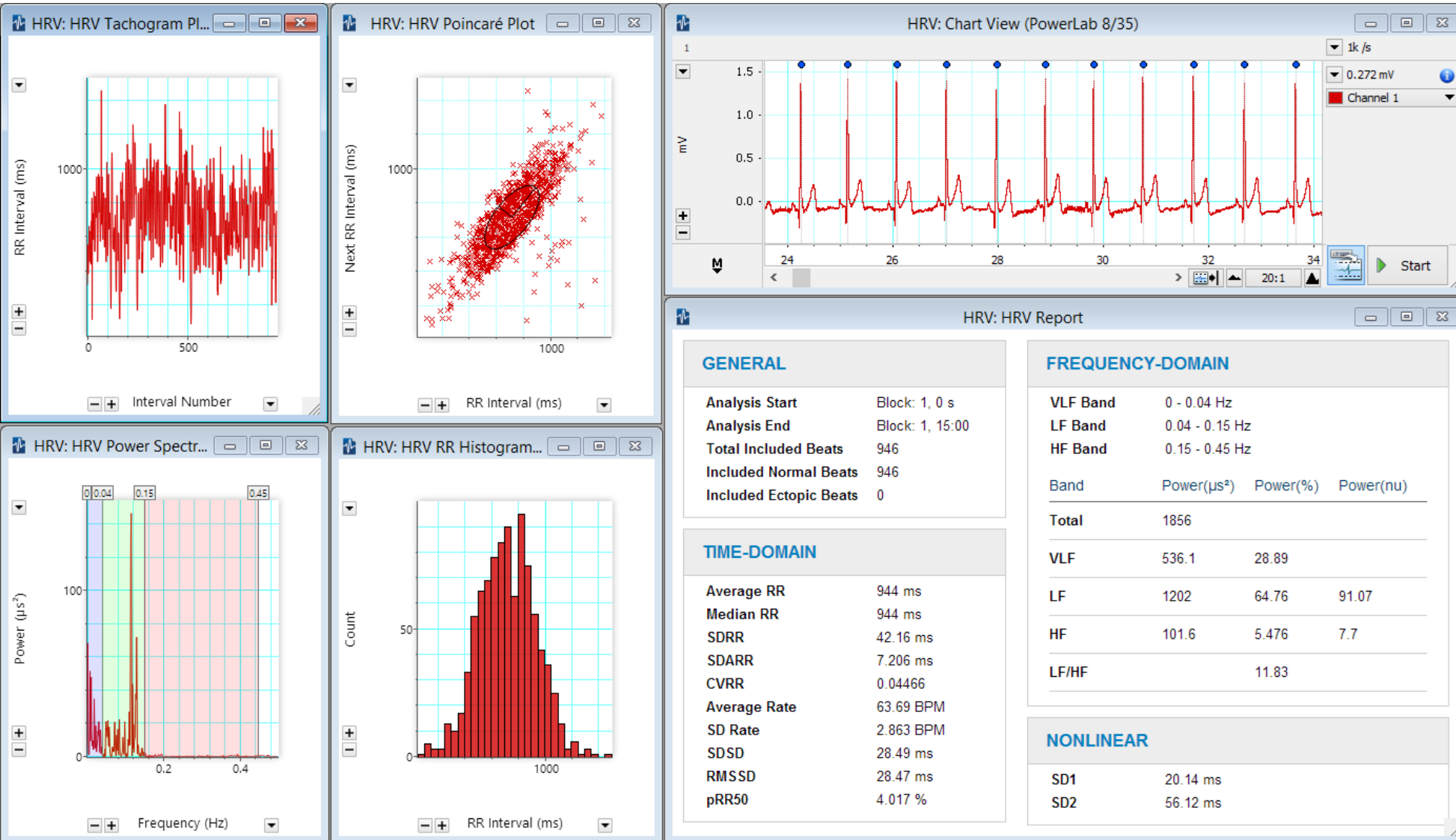


Source: <https://www.istockphoto.com/pl/obrazy/binary-numbers>

Therefore, they are created to implement **mathematical algorithms** in discrete form,
that is: **DSP - Digital Signal Processing** methods → **Features** .



Methods: T, F, T-F signal representation to look at the digital signals from different perspectives
 Heart Rate Variability (HRV) complex example – *how many important diagnostic features can we calculate!*



Source: Original work by the author



Methods: T, F, T-F signal representation to look at the digital signals from different perspectives

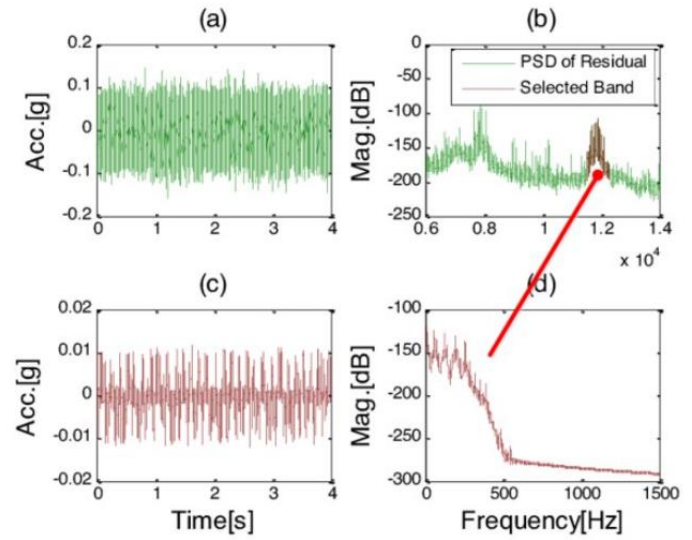
December, 21, 1807

“An arbitrary function, continuous or with discontinuities, defined in a finite interval by an arbitrarily capricious graph can always be expressed as a sum of sinusoids”



Jean B. Joseph Fourier
(1768-1830)

J.B.J. Fourier



Source: Original work by the author

HOW DOES FT WORK ANYWAY?

- Recall that FT uses complex exponentials (sinusoids) as building blocks.
- For each frequency of complex exponential, the sinusoid at that frequency is compared to the signal.
- If the signal consists of that frequency, the correlation is high → large FT coefficients.

$$e^{j\omega t} = \cos(\omega t) + j \sin(\omega t)$$

$$F(\omega) = \int f(t)e^{-j\omega t} dt \quad f(t) = \frac{1}{2\pi} \int F(\omega)e^{j\omega t} d\omega$$

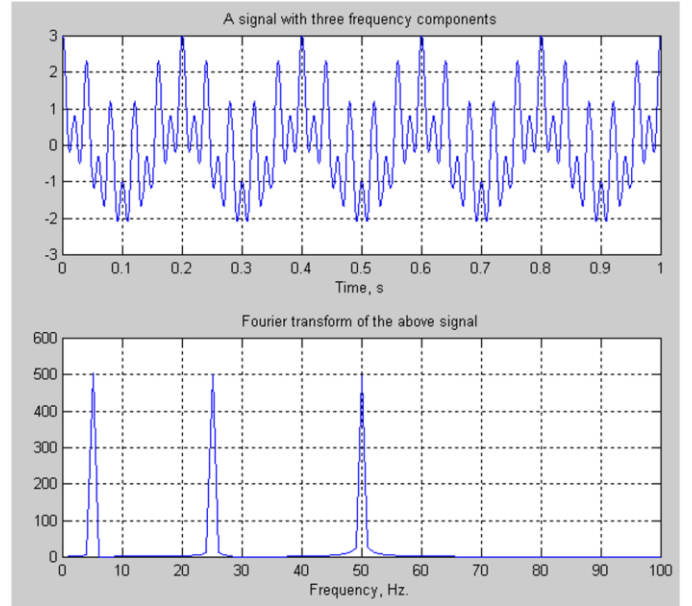
- If the signal does not have any spectral component at a frequency, the correlation at that frequency is low / zero, → small / zero FT coefficient.

$$x_4(t) = \cos(2\pi \cdot 5 \cdot t) + \cos(2\pi \cdot 25 \cdot t) + \cos(2\pi \cdot 50 \cdot t)$$

$$x_4(t) \xleftrightarrow{F} X_4(\omega)$$



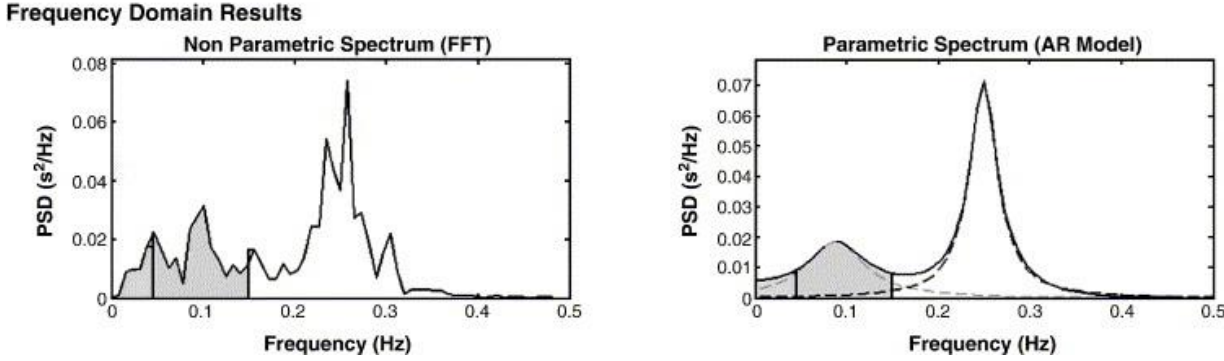
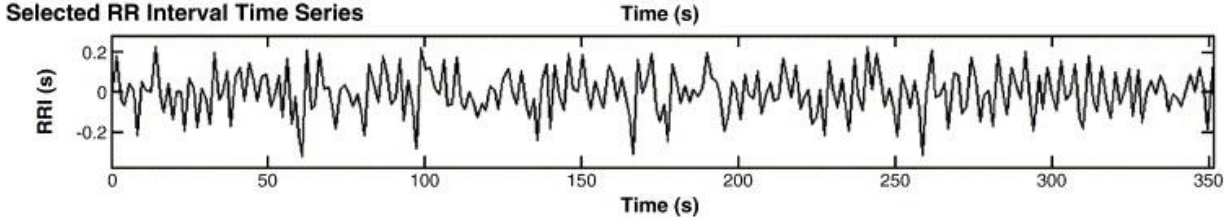
FT AT WORK



Mathematics and (Digital) Signal Processing have been developing for centuries...

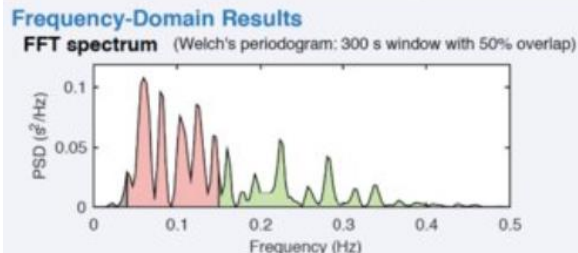
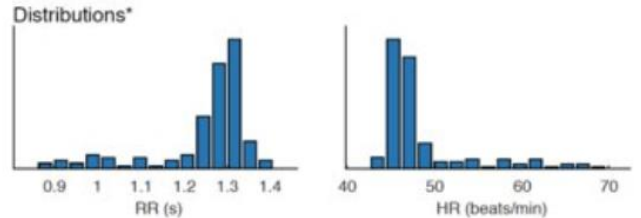
Methods: T, F, T-F signal representation to look at the digital signals from different perspectives

Comparison of time domain and frequency domain HRV signal representation.

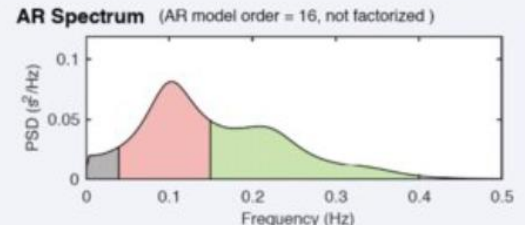


Time-Domain Results

Variable	Units	Value
Mean RR*	(ms)	1248.8
STD RR (SDNN)	(ms)	107.5
Mean HR*	(beats/min)	48.04
Min/Max HR	(beats/min)	44.66/55.30
RMSSD	(ms)	115.7
NNxx	(beats)	69
pNNxx	(%)	47.3
RR triangular index		12,250
TINN	(ms)	401.0



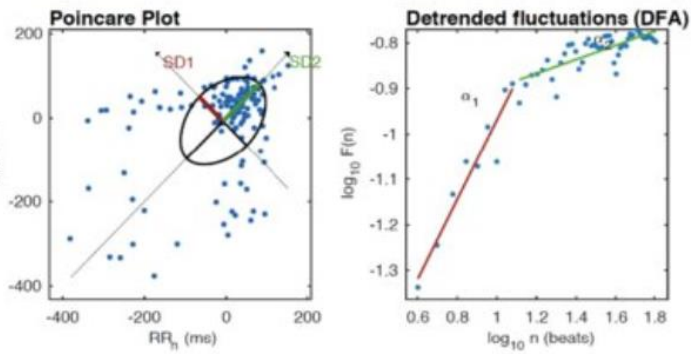
Frequency Band	Peak (Hz)	Power (ms^2)	Power (log)	Power (%)	Power (n.u.)
VLF (0-0.04 Hz)	0.0400	143	4.962	1.7	
LF (0.04-0.15 Hz)	0.0600	5530	8.618	64.4	65.5
HF (0.15-0.4 Hz)	0.2233	2912	7.977	33.9	34.5
Total		8588	9.058		
LF/HF		1.899			



Frequency Band	Peak (Hz)	Power (ms^2)	Power (log)	Power (%)	Power (n.u.)
VLF (0-0.04 Hz)	0.0400	877	6.777	6.5	
LF (0.04-0.15 Hz)	0.1033	6475	8.776	48.1	51.5
HF (0.15-0.4 Hz)	0.1500	6100	8.716	45.3	48.5
Total		13459	9.507		
LF/HF		1.061			

Nonlinear Results

Variable	Units	Value
Poincare Plot		
SD1	(ms)	82.1
SD2	(ms)	125.9
SD2/SD1		1.533
Approximate Entropy (ApEn)		0.839
Sample Entropy (SampEn)		1.293
Detrended Fluctuation Analysis (DFA)		
Short-term fluctuations, α_1		0.876
Long-term fluctuations, α_2		0.154



<https://www.sciencedirect.com/science/article/abs/pii/S0022073605002293>



Methods: T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform

THE WAVELET TRANSFORM

- Overcomes the preset resolution problem of the STFT by using a variable length window
- Analysis windows of different lengths are used for different frequencies:
 - ↳ Analysis of high frequencies → Use narrower windows for better time resolution
 - ↳ Analysis of low frequencies → Use wider windows for better frequency resolution
- This works well, if the signal to be analyzed mainly consists of slowly varying characteristics with occasional short high frequency bursts.
- Heisenberg principle still holds!!!
- The function used to window the signal is called *the wavelet*

THE WAVELET TRANSFORM

Translation parameter, measure of time Scale parameter, measure of frequency A normalization constant Signal to be analyzed

$$CWT_x^\psi(\tau, s) = \Psi_x^\psi(\tau, s) = \frac{1}{\sqrt{|s|}} \int_t x(t) \psi^* \left(\frac{t - \tau}{s} \right) dt$$

Continuous wavelet transform of the signal $x(t)$ using the analysis wavelet $\psi(\cdot)$

The mother wavelet. All kernels are obtained by translating (shifting) and/or scaling the mother wavelet

Scale = 1/frequency

Methods: T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform

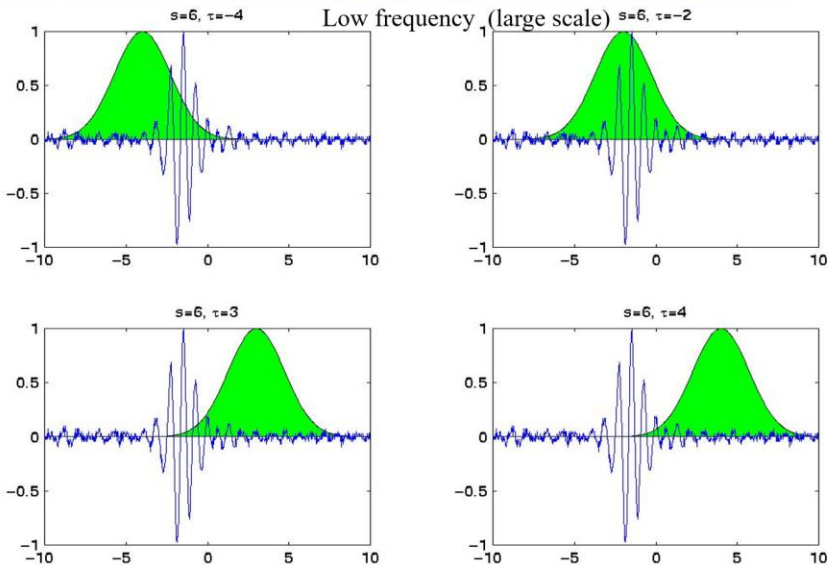
The wavelet transform is like a **microscope** with adjustable focus:

➤ **to see both "forest" and "trees"**

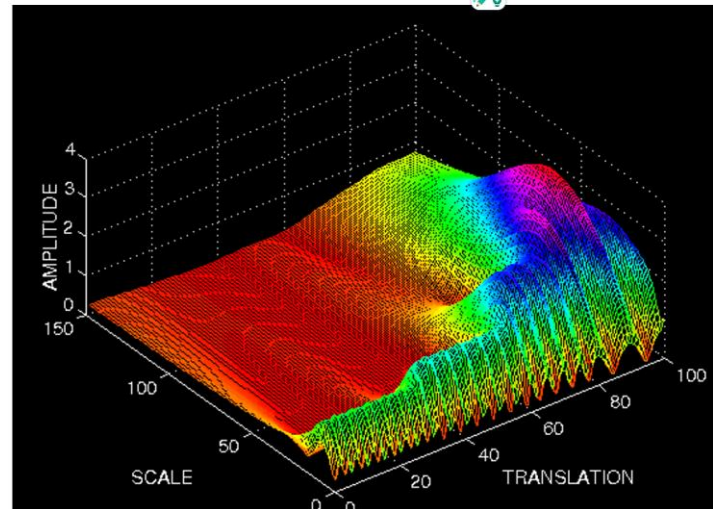


$$CWT_x^\psi(\tau, s) = \Psi_x^\psi(\tau, s) = \frac{1}{\sqrt{|s|}} \int_{-\infty}^{\infty} x(t) \psi^* \left(\frac{t-\tau}{s} \right) dt$$

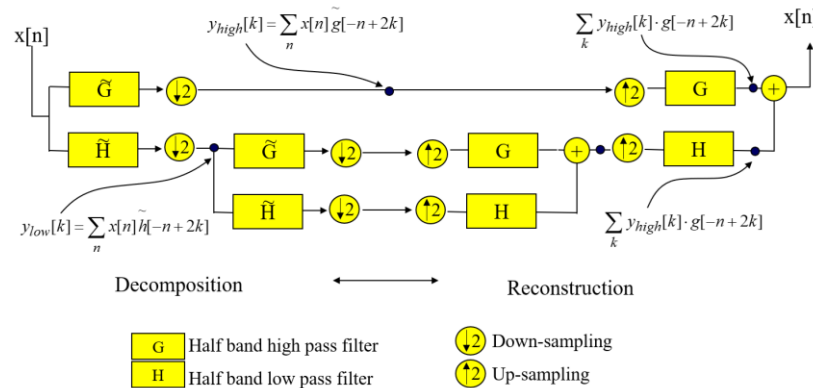
WT AT WORK



WT AT WORK



DISCRETE WAVELET TRANSFORM IMPLEMENTATION



2-level DWT decomposition. The decomposition can be continued as long as there are enough samples for down-sampling.



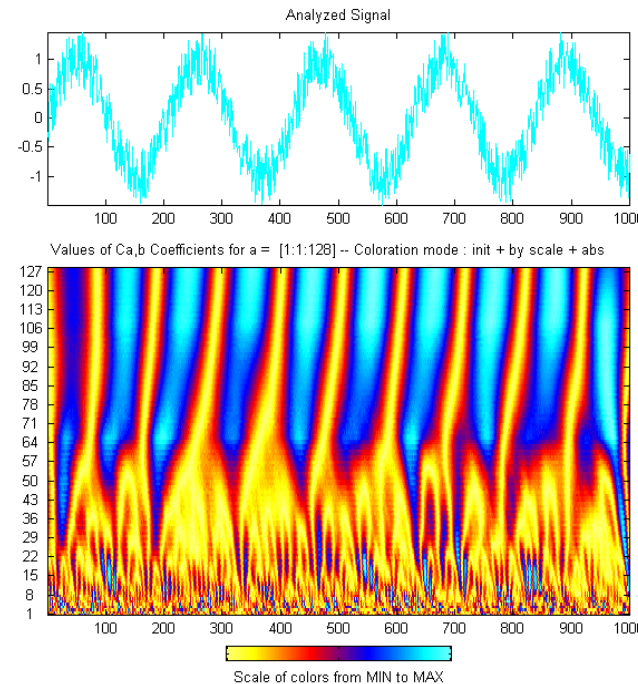
Development of the wavelet-neural systems (WNS) for classification and identification of chosen biomedical events.

Paweł Kostka, Ph.D. project: 1996-2000,

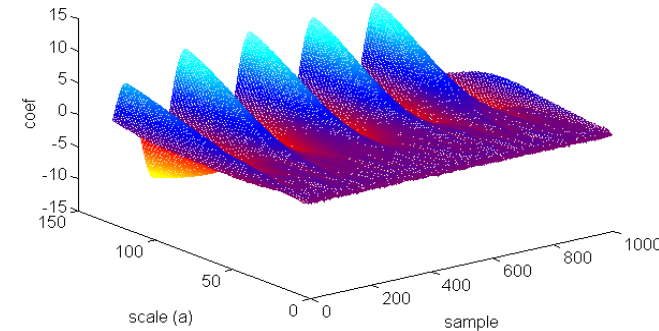
Promoter: prof. Ewaryst Tkacz



prof. Ewaryst Tkacz



WT signal decomposition examples.



Methods & case: T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform for HRV analysis.

An improvement of unsupervised hybrid biomedical signal classifiers by optimal feature extraction in system preliminary layer .

Pawel Kostka, Ewaryst Tkacz

*Silesian University of Technology, Institute of Electronics
Division of Biomedical Electronics
Gliwice, Poland*

26th Annual International Conference
IEEE Engineering in Medicine and Biology Society (EMBS)
September 1-5, 2004, San Francisco California.

HYBRID SYSTEMS

- Hybrid systems combine different Artificial Intelligence (AI) methods:
 - Neural Networks
 - Genetics Algorithms
 - Fuzzy Sets
 - Other signal processing methods

to be able do deal with complex biomedical systems.

GENERAL STRUCTURE OF WAVELET – NEURAL SYSTEM



- QRS detection
- HRV signal calculation
- Cont. represent. of HRV (DCSI)
- Resampling (fs = 5 [Hz])



Source: Original works by the author

Methods & case 😊: T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform for HRV analysis.

New feature vector creation

Energy of wavelet component

$$E_{1,j}\{c_{i,j}\} = (c_{i,j})^2 \Rightarrow E_{1,j}\{s(n)\} = \sum_i (c_{i,j})^2$$

The (non-normalized) Shannon entropy:

$$E_{2,j}\{c_{i,j}\} = -(c_{i,j})^2 \log(c_{i,j})^2 \Rightarrow E_{2,j}\{s(n)\} = -\sum_i [(c_{i,j})^2 \log(c_{i,j})^2]$$

The concentration in l^p norm with $1 < p < 2$.

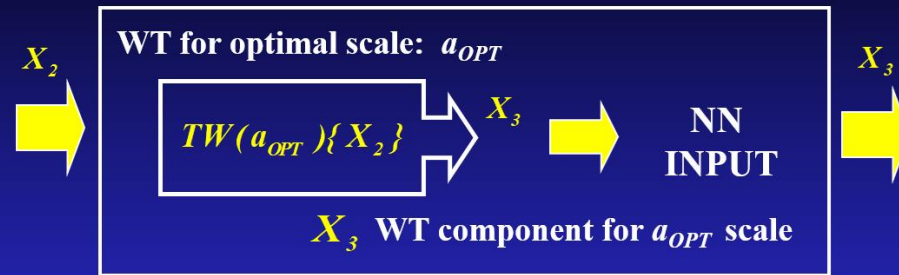
$$E_{3,j}\{c_{i,j}\} = |c_{i,j}|^p \Rightarrow E_{3,j}\{s(n)\} = \sum_i |c_{i,j}|^p = \|s(n)\|_p^p$$

The logarithm of the “energy” entropy.

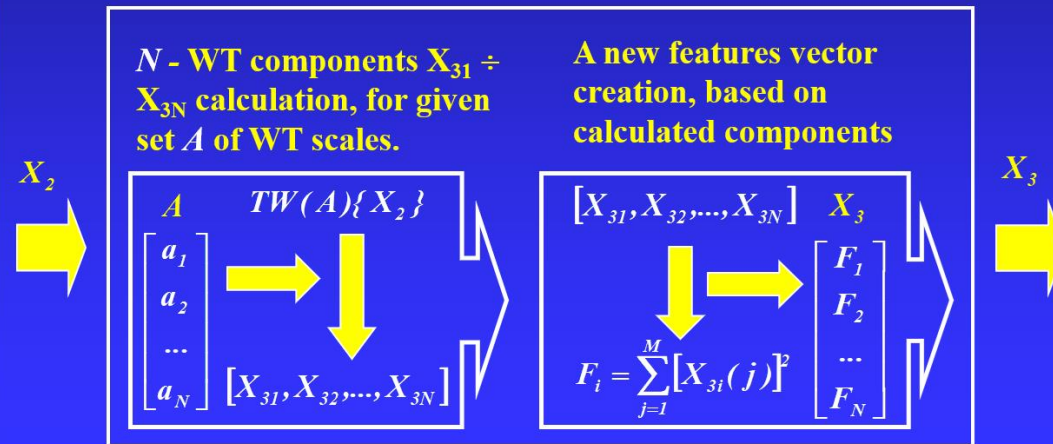
$$E_{4,j}\{c_{i,j}\} = \log(c_{i,j})^2 \Rightarrow E_{4,j}\{s(n)\} = \sum_i \log(c_{i,j})^2$$

LEARNING ALGORITHM OF WAVELET LAYER (SCALE – a) STRUCTURE OF TWO DIFFERENT WAVELET LAYERS

WAVELET LAYER - TYPE I

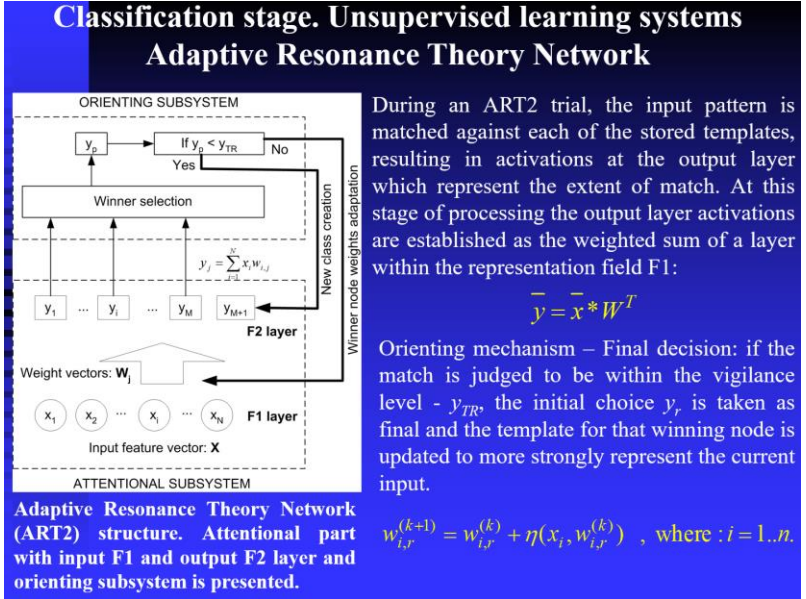
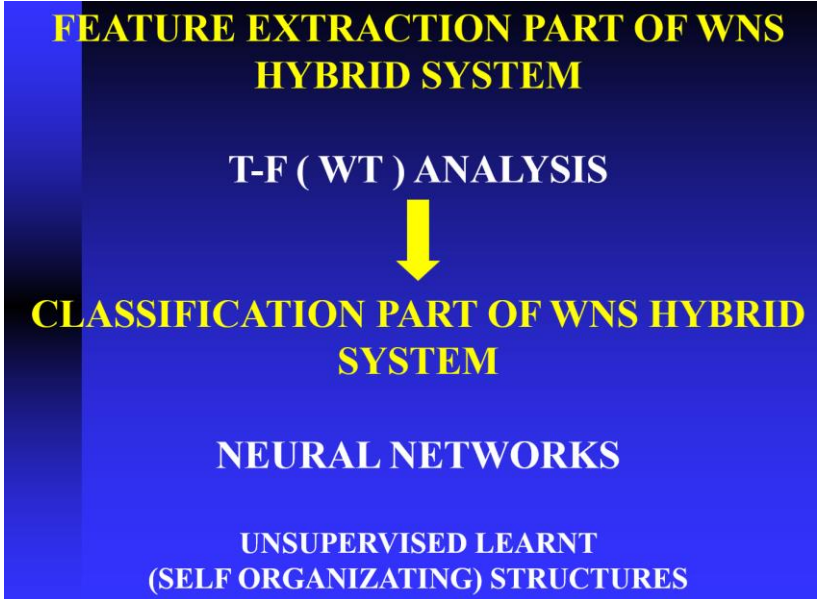
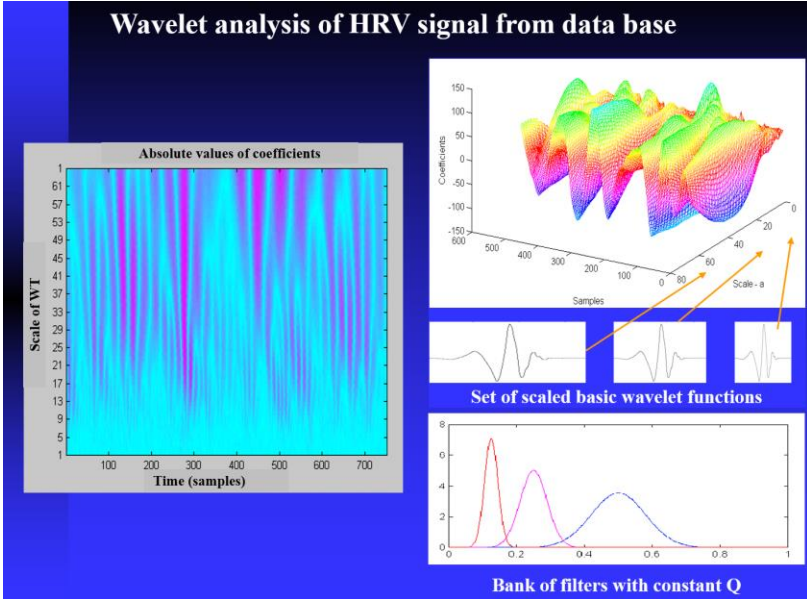


WAVELET LAYER - TYPE II



Methods & case: T, F, T-F signal representation to look at the digital signals from different perspectives

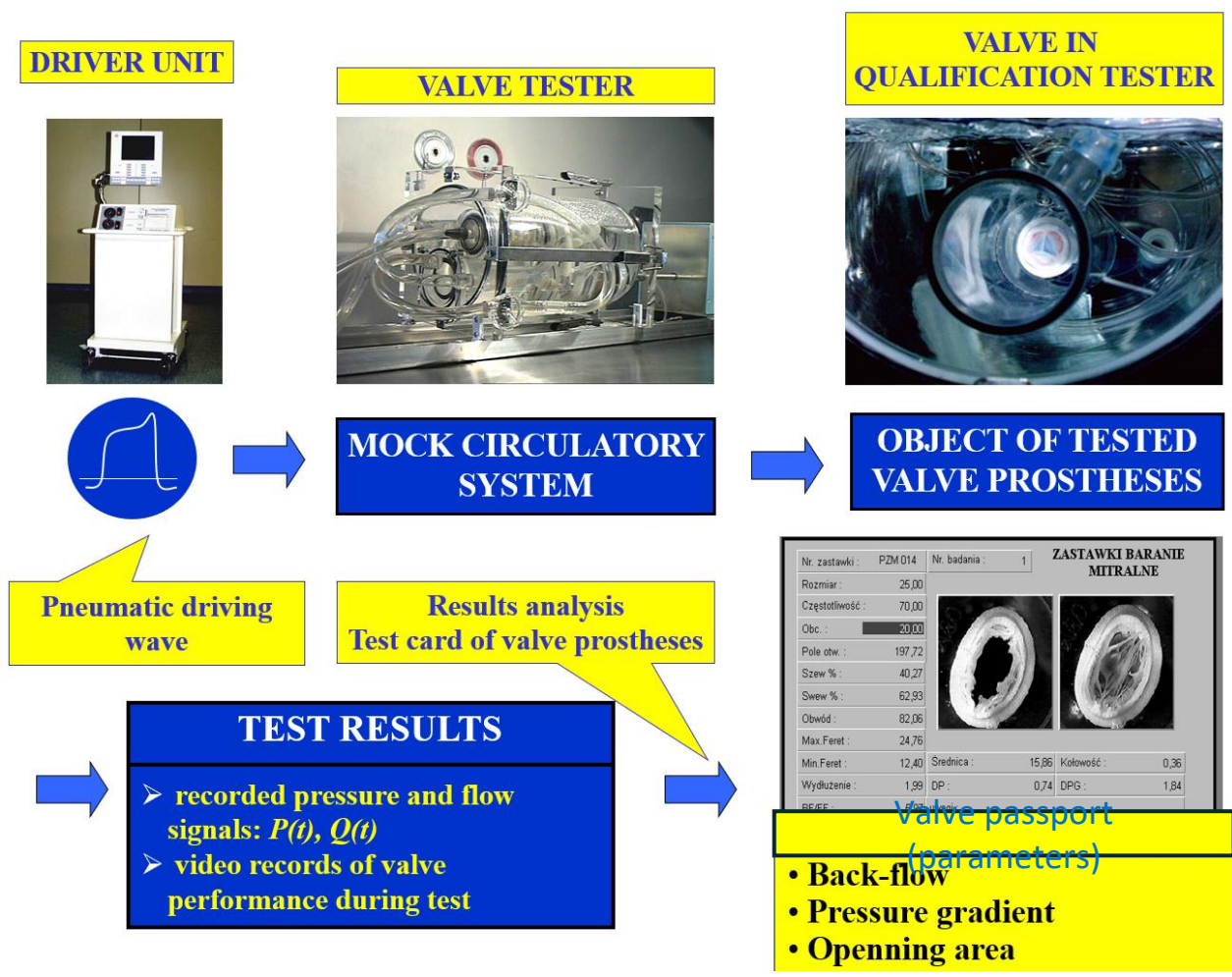
T-F hybrid representation employing the Wavelet Transform for HRV analysis of patients with Coronary Artery Disease.



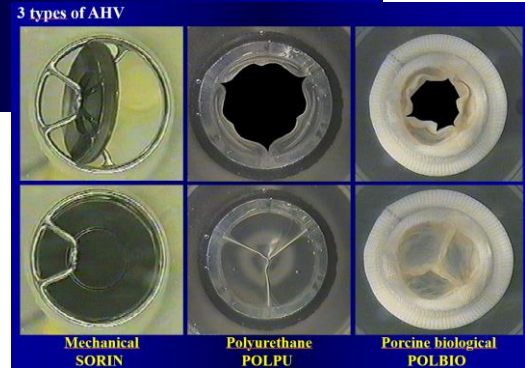
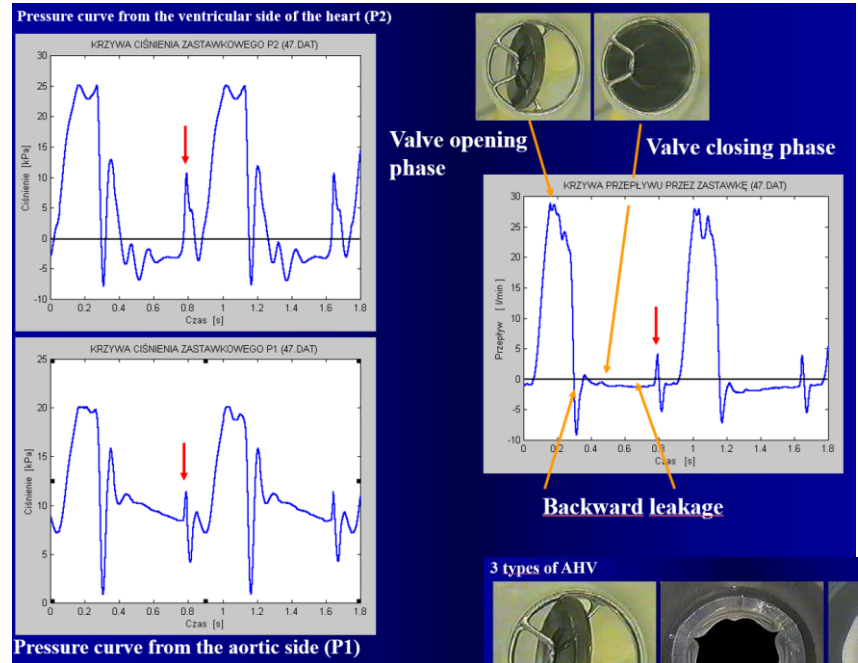
Methods & case : T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform for biomedical curves modeling.

Case: Modelling of the Heart Valve Prostheses (HVP) Flow Q , based on pressures: P_{IN} & P_{OUT} during valve test.



ZASTAWKI BARANIE MITRALNE	
Nr. zastawki:	PZM 014
Nr. badania:	1
Rozmiar:	25,00
Częstotliwość:	70,00
Obc.:	20,00
Pole otw.:	197,72
Szew %:	40,27
Swew %:	62,93
Obwód:	82,06
Max.Feret:	24,76
Min.Feret:	12,40
Wydłużenie:	1,99
DP:	0,74
DPG:	1,84

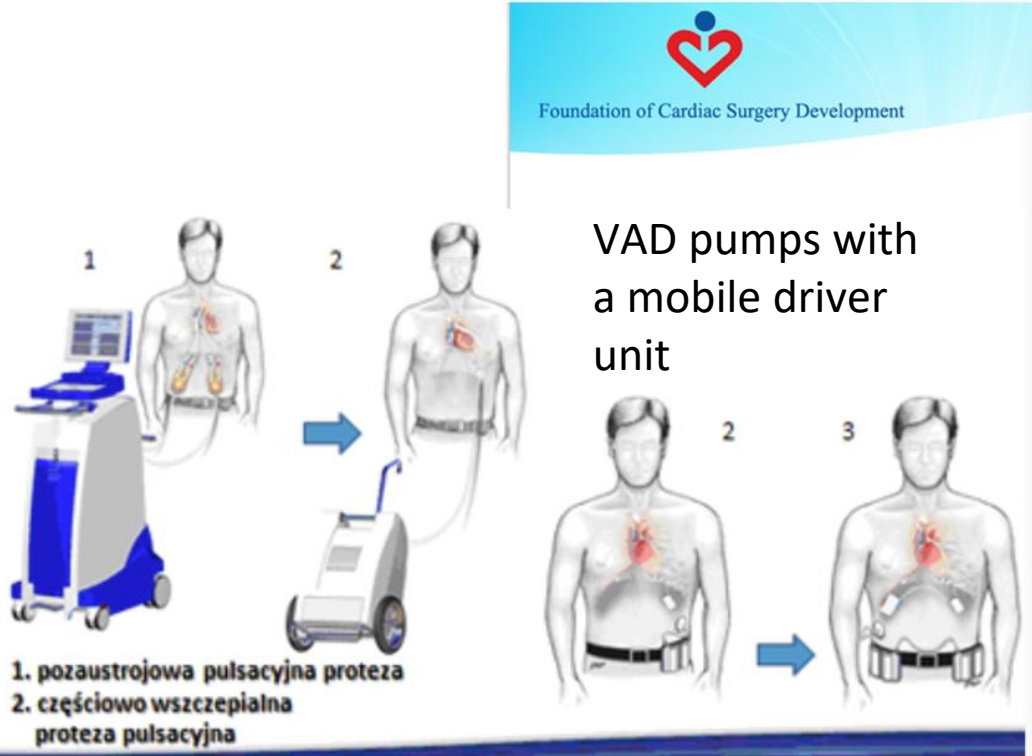


Source: Original works by the author

Methods & case 😊: T, F, T-F signal representation to look at the digital signals from different perspectives

T-F hybrid representation employing the Wavelet Transform for detection of characteristic points of VAD control curves.

Institute of Heart Prostheses (Foundation for Cardiac Surgery Development)



The Artificial Heart Laboratory of Heart Prostheses Institute Foundation of Cardiac Surgery Development



Source: www.frk.pl



Ventricular Assist Device (VAD) as a bridge to transplantation

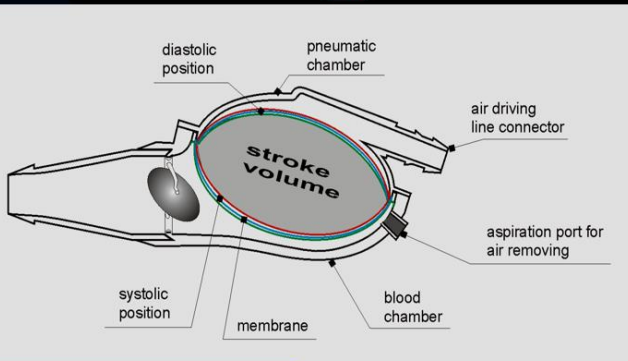


Methods & case 😊: T, F, T-F signal representation to look at the digital signals from different perspectives

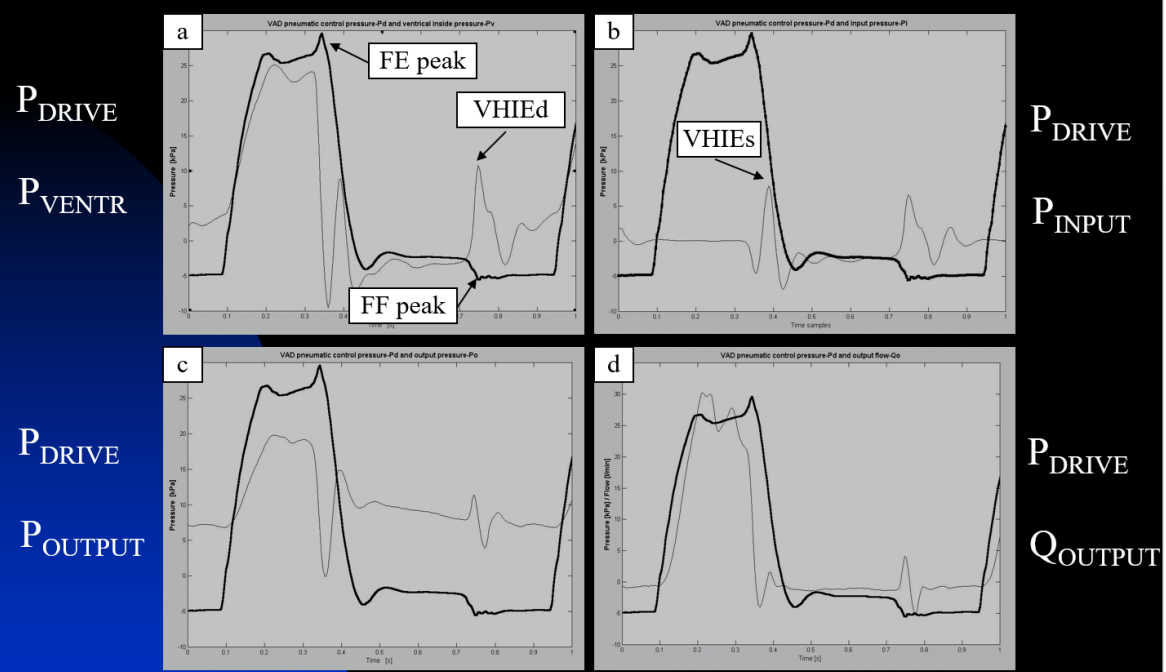
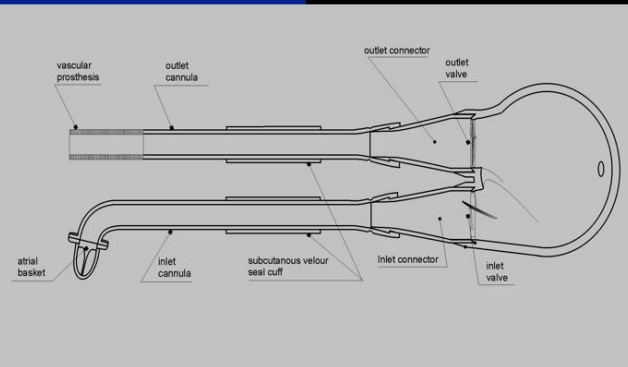
T-F hybrid representation employing the Wavelet Transform for detection of characteristic points of VAD control curves.

It is very important in the VAD control process (*the hydraulic pump is controlled by a pneumatic wave - compressible*)

VENTRICULAR ASSIST DEVICE POL-VAD



- Pneumatically driven membrane blood pump
- Mechanical, disc valves Sorin-Biomedica were placed in inlet and outlet channels
- Both VAD walls and membrane are made of bio-compatible polyurethane



FE – state of chamber full ejection, at the end of systolic cycle phase.
FF – state of chamber full fill, at the end of diastolic cycle phase
VHIE – ventricular hemodynamical inertial effect, which is also called as “hydraulic hammer” can be seen as a characteristic pressure and flow wave caused by sudden membrane stopping after systolic FE (VHIEs) or diastolic FF (VHIEd) phases.

Methods & case 😊: T, F, T-F signal representation to look at the digital signals from different perspectives

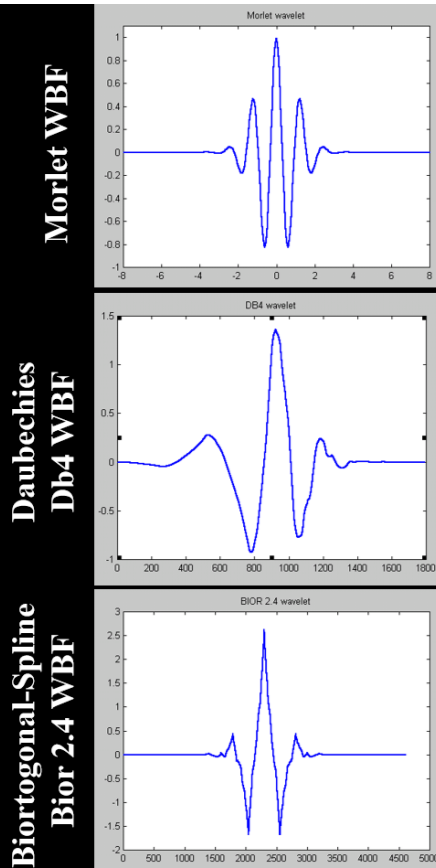
T-F hybrid representation employing the **Wavelet Transform** for detection of characteristic points of VAD control curves.

It is very important in the VAD control process (*the hydraulic pump is controlled by a pneumatic wave - compressible*)

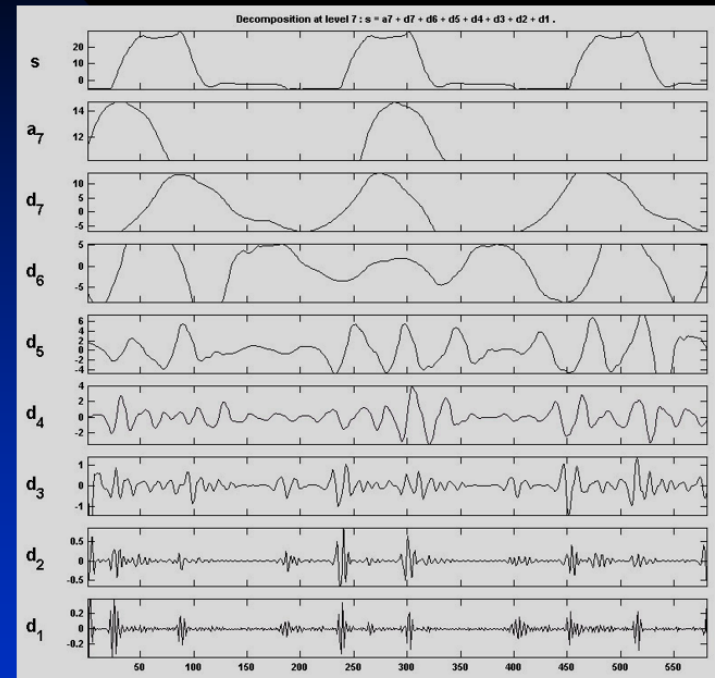
Wavelet Transform → Basic function selection

Main features of WBF:

- Ortogonality
- Biortogonality
- Compact support
- Symmetry
- Regularity and smoothness
- Number of vanishing moments
- Analytical formula of basic function
- Interpolation
- Rational coefficients



MULTILEVEL, WAVELET DECOMPOSITION OF VAD DRIVEN SIGNAL P_D , ACCORDING TO MALLAT ALGORITHM.



FREQUENCY SUB-BANDS RANGE

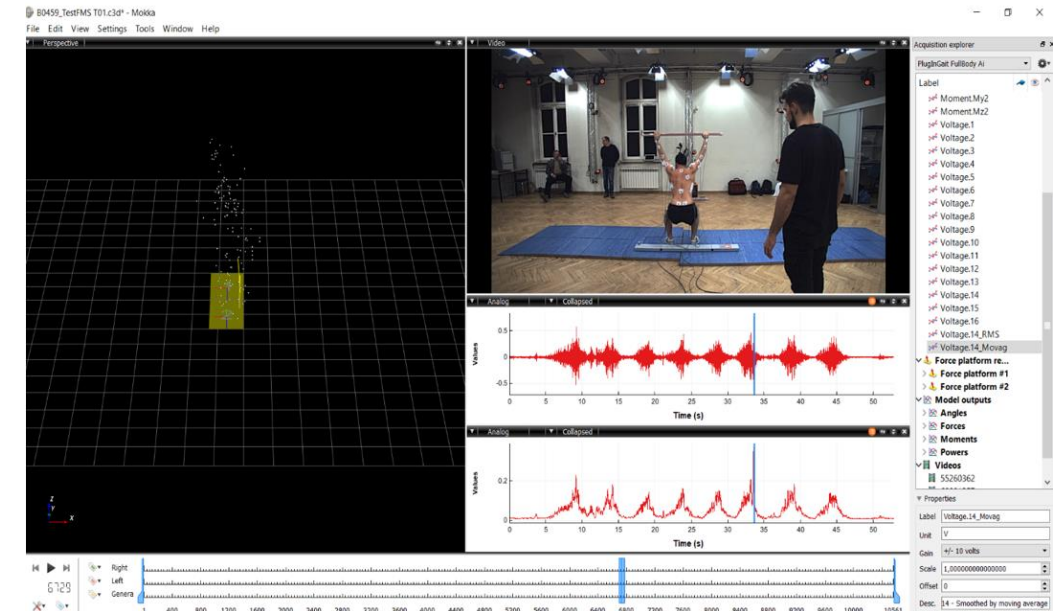
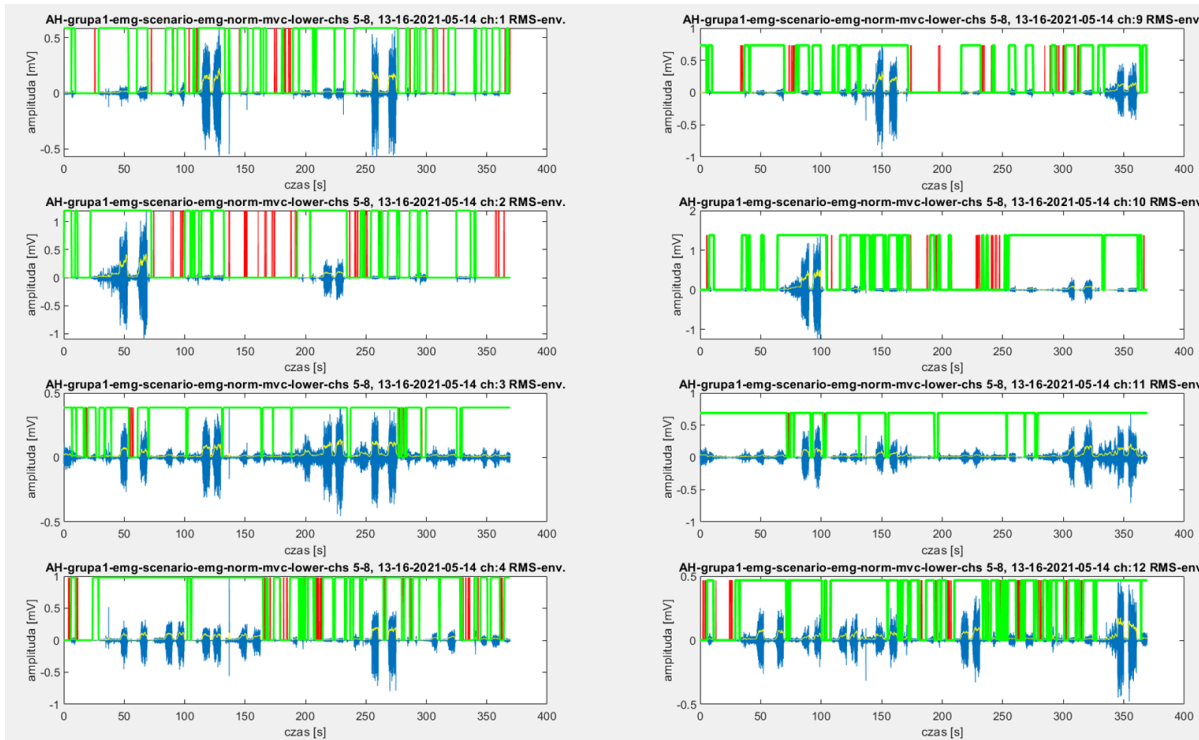
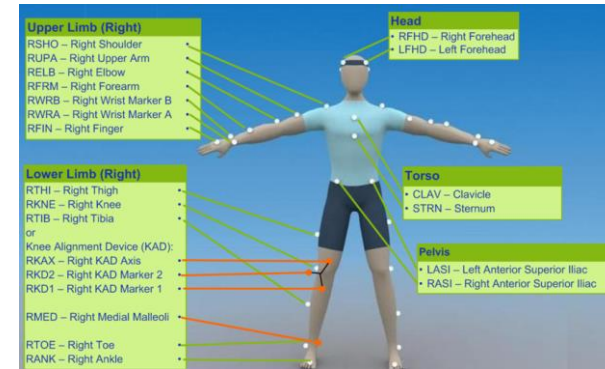
(based on frequency analysis of pressure and flow signals)

- d_2 : 31.25 ÷ 62.5 [Hz]
- d_3 : 15.63 ÷ 31.25 [Hz]
- d_4 : 7.81 ÷ 15.63 [Hz]
- d_5 : 3.90 ÷ 7.81 [Hz]
- d_6 : 1.95 ÷ 3.90 [Hz]
- d_7 : 0.98 ÷ 1.95 [Hz].

Use case (Each of the following cases is a separate story 😊 and project) :

EMG(t) signal on-line analysis from real-time measurements, during the examination of a group of professional athletes. **Toward predictive detection of possible injury.**

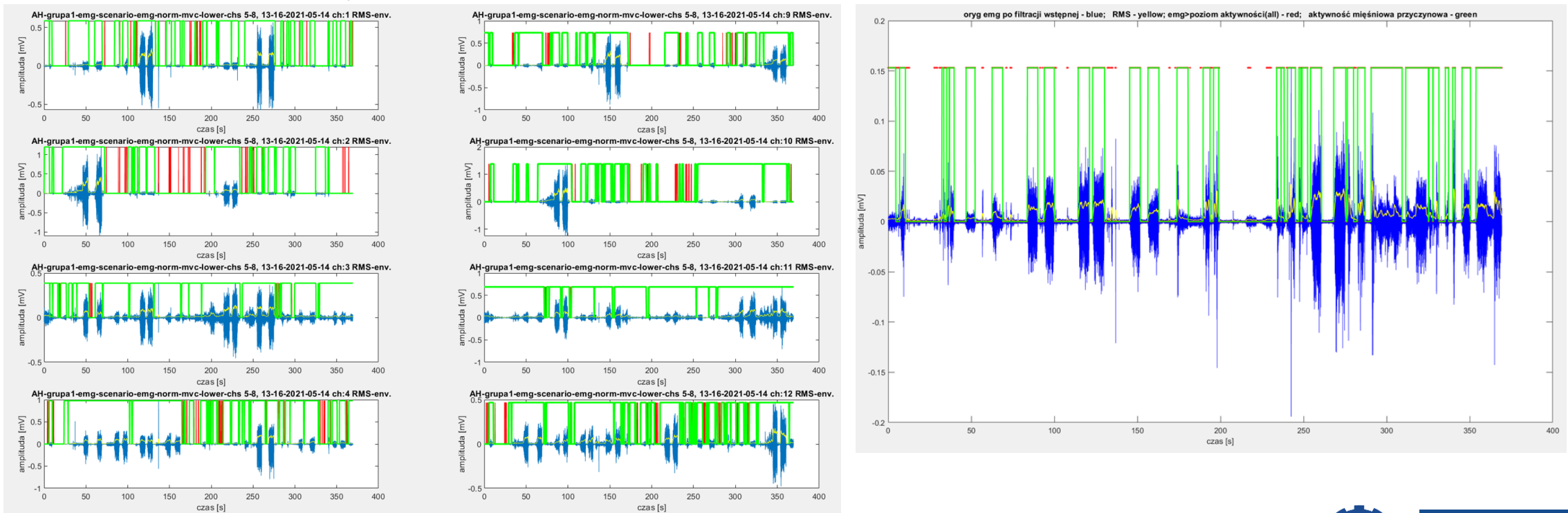
- T, F, T-F multimodal biomedical signal processing,
- emg(t) filtration with an optimized filter cascade;
- development of an algorithm for determining causal muscle activity;



Use case (Each of the following cases is a separate story 😊 and project) :

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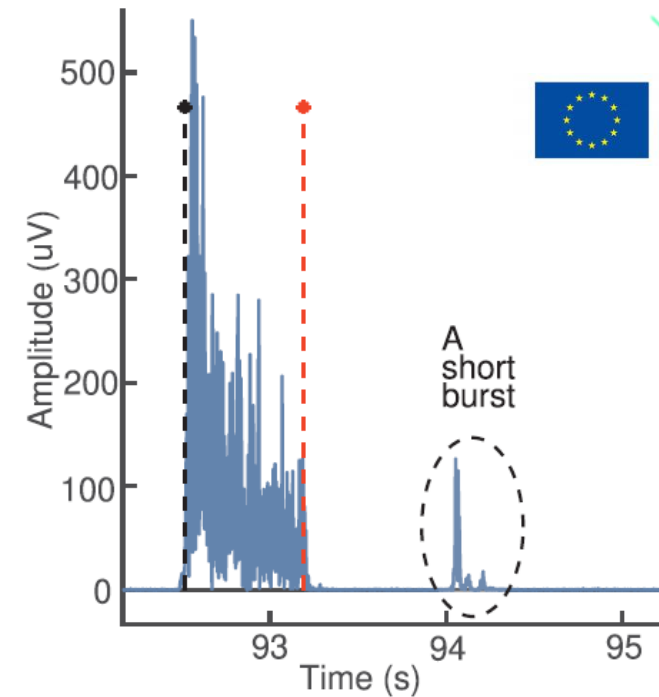
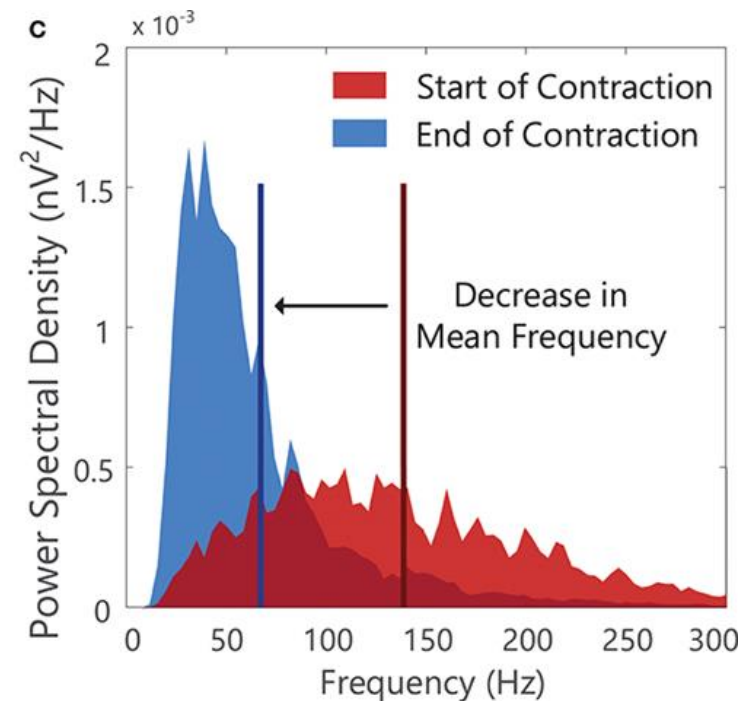
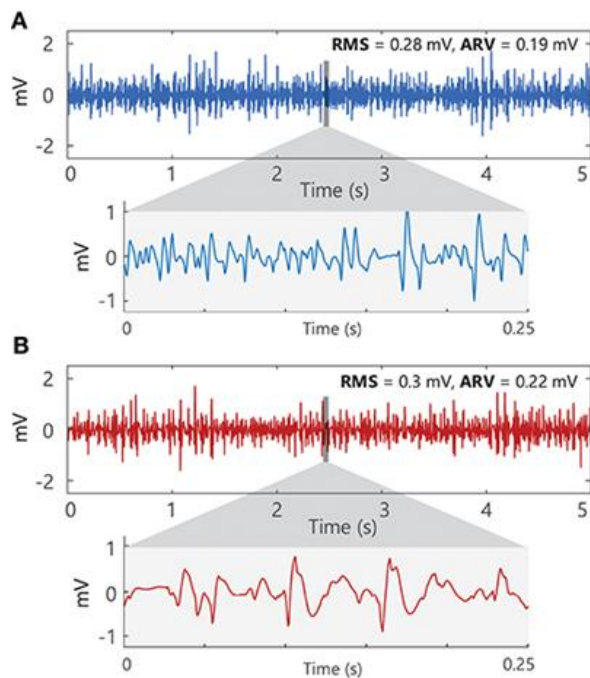
- T, F, T-F multimodal biomedical signal processing,
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Use case:

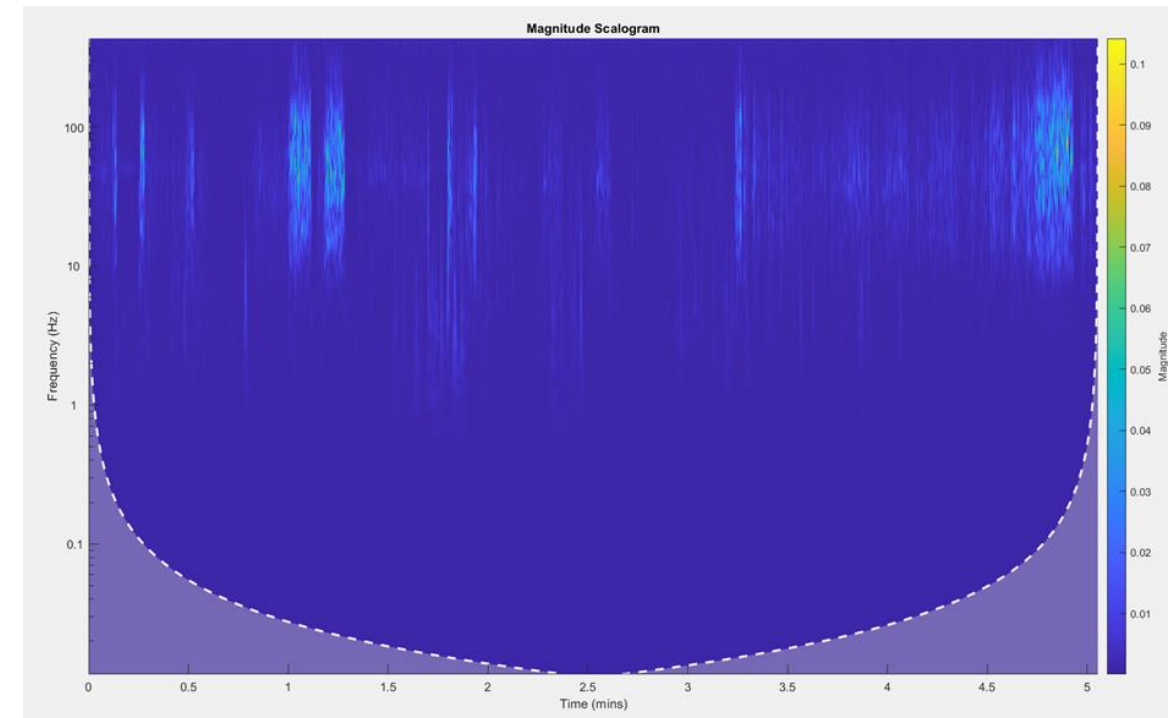
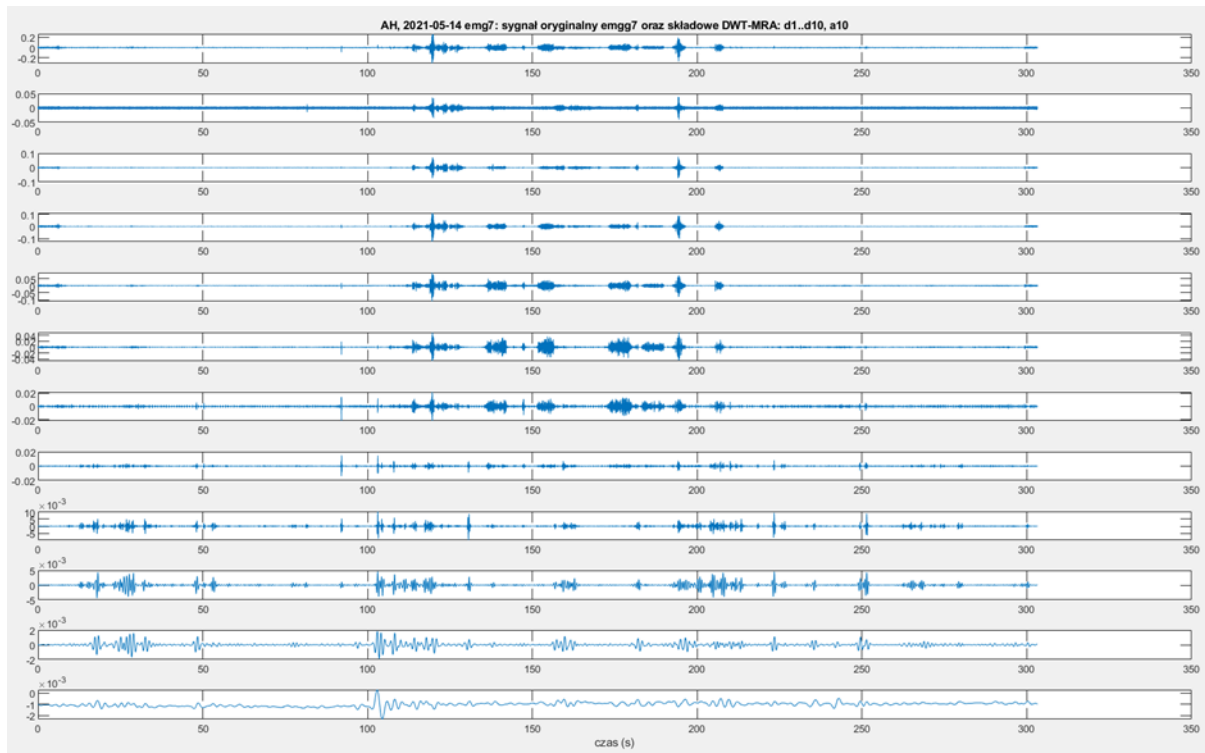
EMG(t) signal on-line analysis from real-time measurements, during the examination of a group of professional athletes. *Toward predictive detection of possible injury.*

- burst artefacts (,outliers') removal;
- frequency analysis of emg(t) in activation state;



Use case:

- T-F wavelet emg(t) signal analysis;
- multi-level DWT signal decomposition;
- *db4, bior 2.4, 3.5, symlet6 – wavelet;*



AH, 2021-05-14, lower MVC, emg7(t)

Levels	energy_by_scales	
{'D1' }	1.4845	energy_total =
{'D2' }	2.1464	
{'D3' }	5.6277	
{'D4' }	8.7217	
{'D5' }	4.9273	
{'D6' }	1.2118	
{'D7' }	0.39971	
{'D8' }	0.38503	
{'D9' }	0.2369	
{'D10' }	0.044175	
{'A10' }	0.32305	
		<u>25.508</u>

Use case

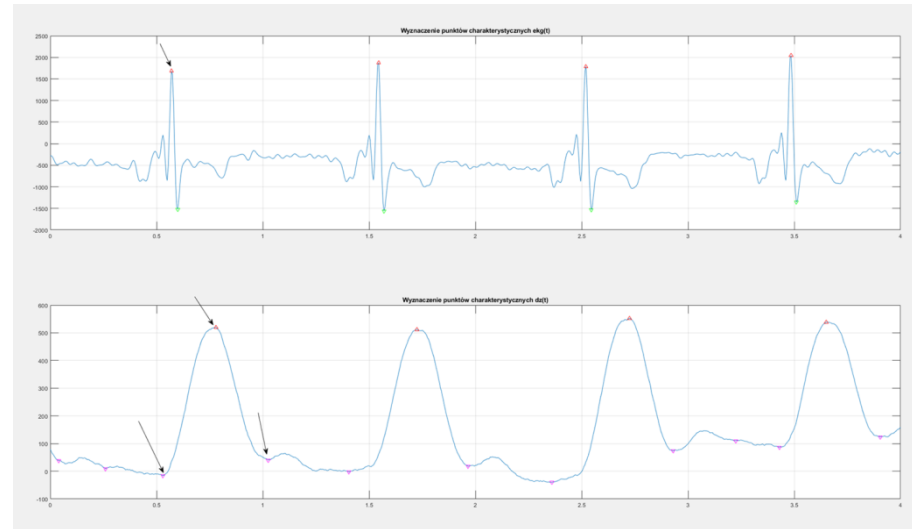
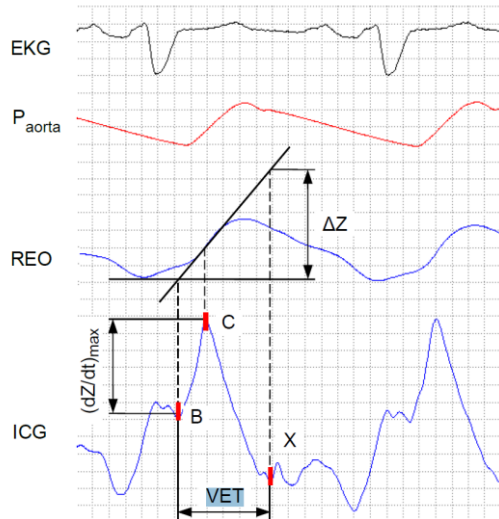
(Stroke volume & Cardiac output estimation from $ecg(t)$ & $Z(t)$ altern. for USG):

Relevant diagnostic features extraction from **multimodal, multichannel biomedical signal measurement systems** using sophisticated digital signal processing (DSP) methods developed in the time (T), frequency (F), and hybrid T-F domains.

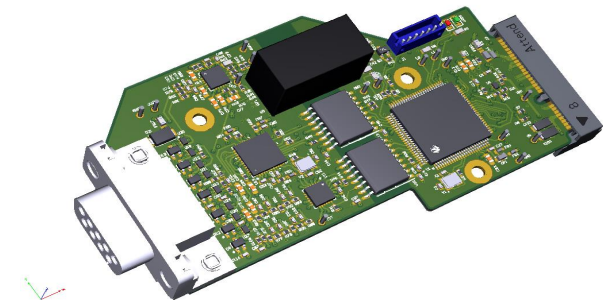
Stroke volume (SV) estimation, based on non-invasive, widely accessible $ecg(t)$ & $Z(t)$ signals

from Kubicek formula:

$$SV = \rho * \left(\frac{L}{Z_0}\right)^2 * \left(\frac{dZ}{dt}\right)_{max} * t_{VET} \quad [cm^3 = ml]$$



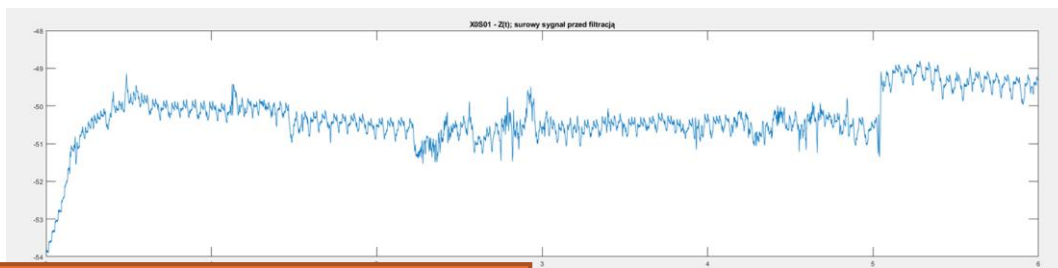
Custom design of multimodal – multichannel biomedical data acquisition system for $ecg(t)$ & $Z(t)$



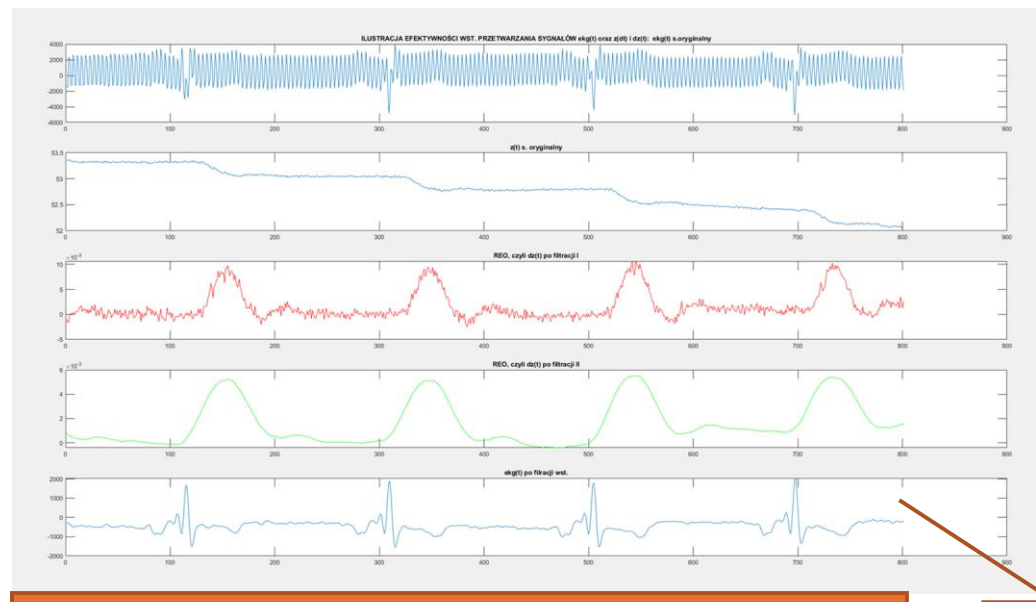
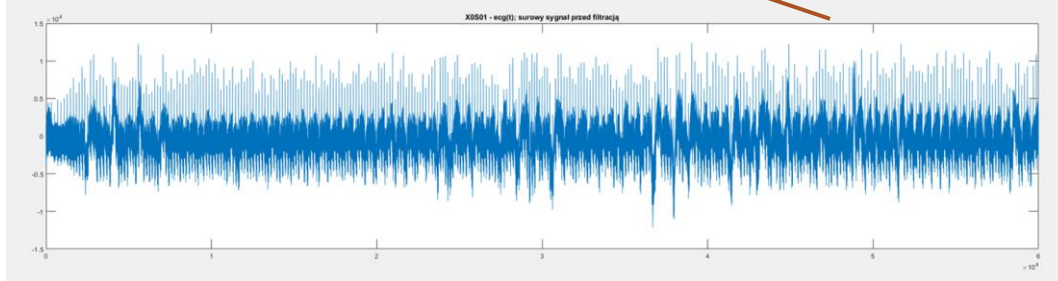
Use cases:

Estimation of Stroke Volume (SV) and Cardiac Output ($=SV \cdot HR$) based on non-invasive, widely accessible ECG(t) and Z(t) signals.

Effect of raw, noisy input signals
,cleaning' using developed DSP methods (filter banks)



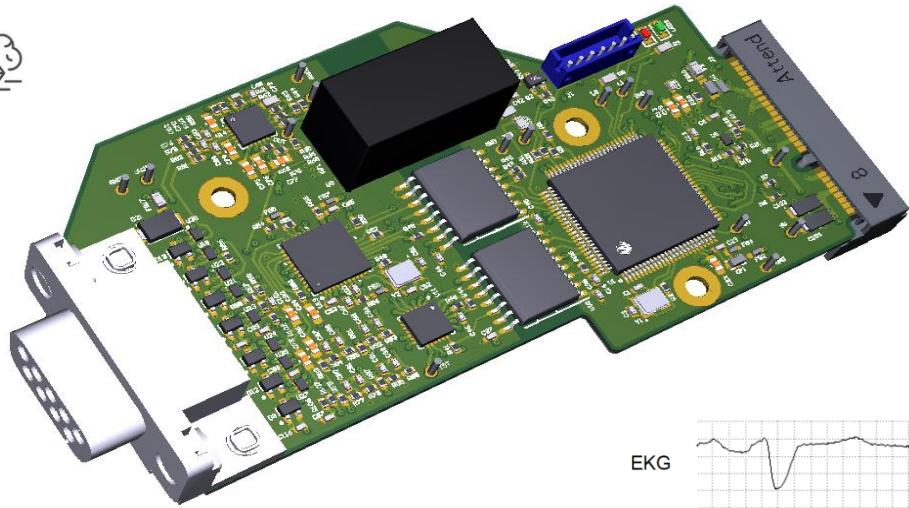
raw registered signals: ecg(t) & Z(t)



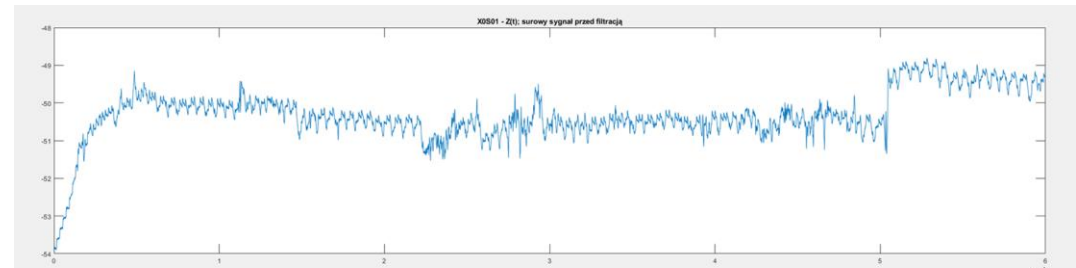
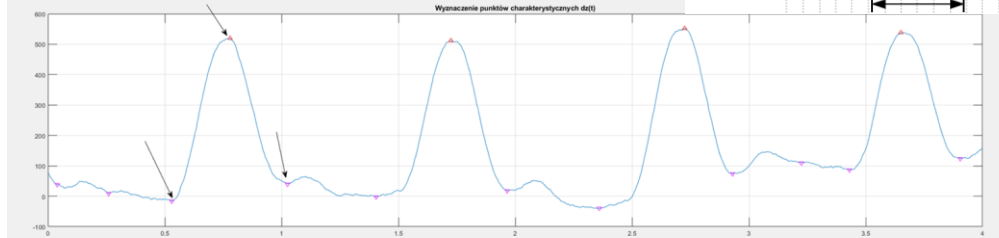
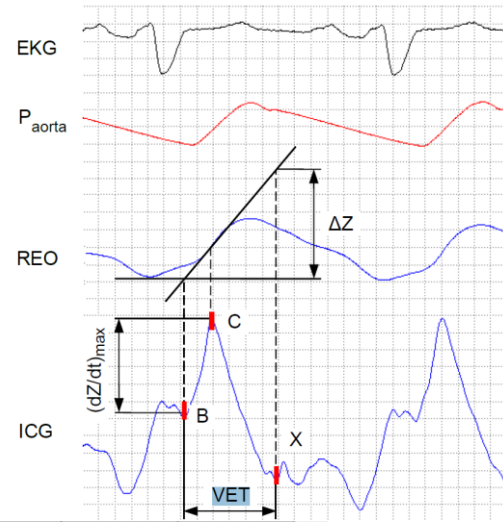
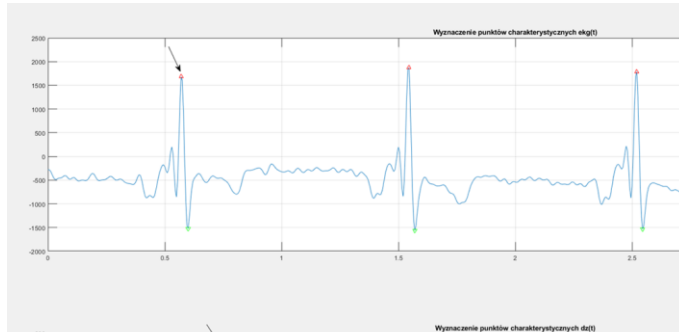
The same „cleaned’ signals after our DSP algorithms

Our research: from raw data to diagnostic data & knowledge

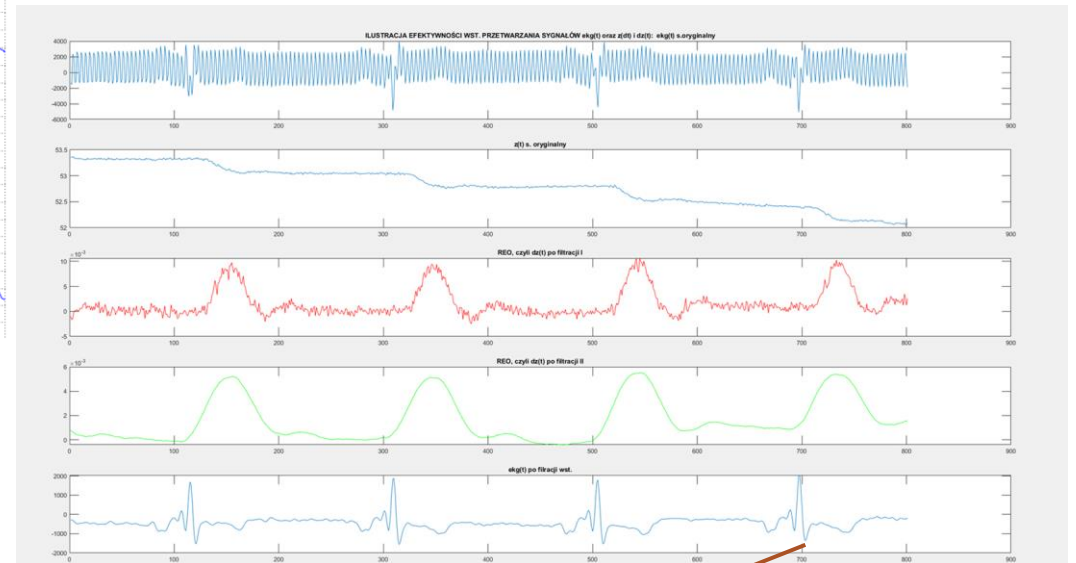
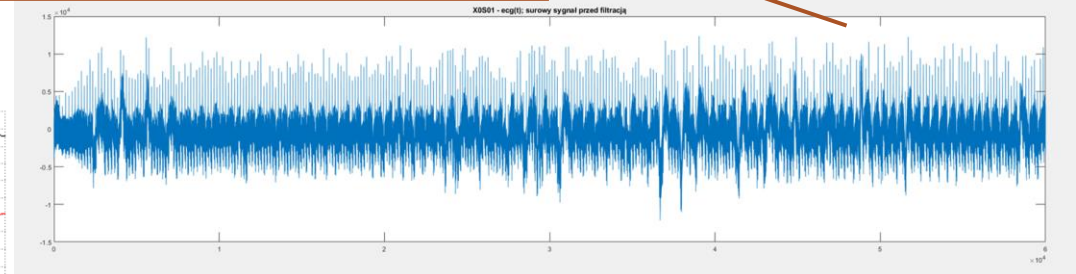
„REO” project results: hardware & biomed. data processing



custom design of multimodal – multichannel biomedical data registration system



raw registered signals: $ecg(t)$ & $Z(t)$

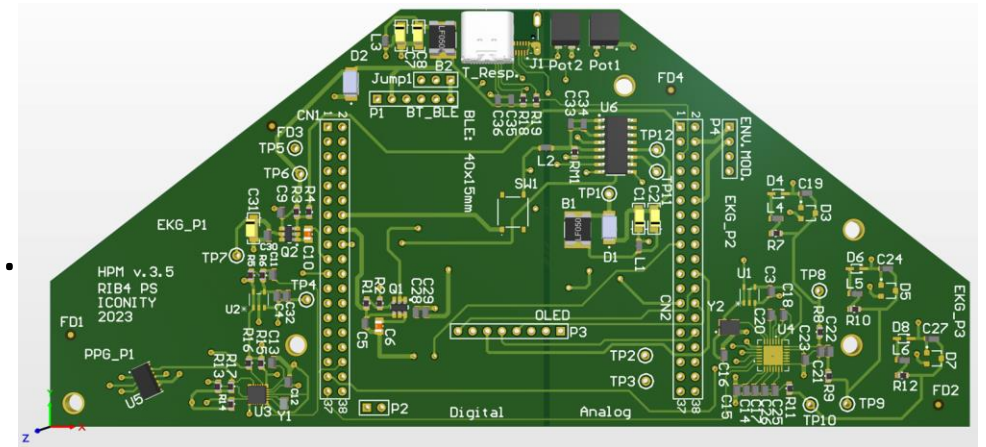
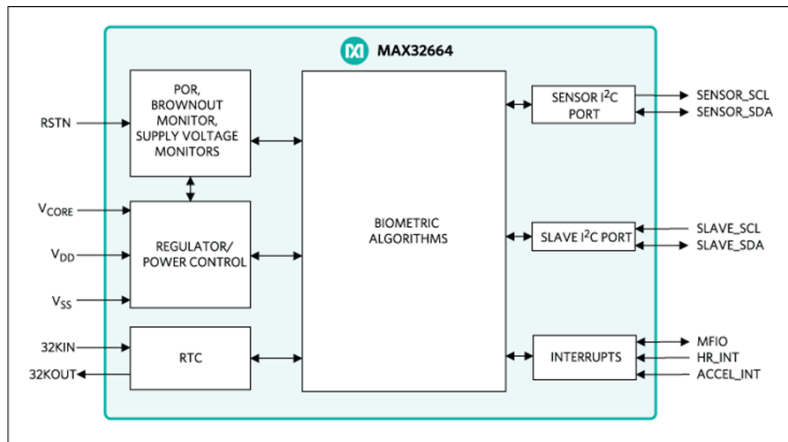


„cleaned” signals after our DSP algorithms

Use case: Design of a system for recording & processing physiological signals, including the respiratory curve at home (*from hospital to home idea*) - integrated with the measurement of environmental parameters.

In a hardware domain, the state-of-the-art personalized data acquisition systems was developed, by means of System on Integrated Chip (SoIC) type systems: Analog Front-End (AFE) chips.

- Use of the modern AFE's SOiC systems, including Ultralow Power Biometric Sensor Hub: MAX32664 integrated with other specialized AFEs.

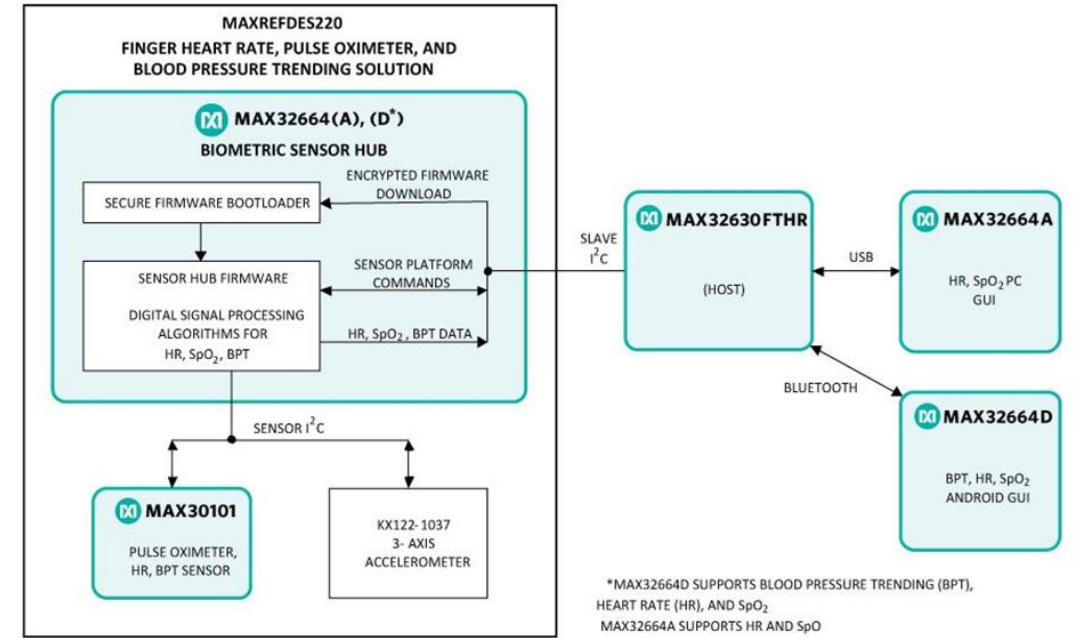
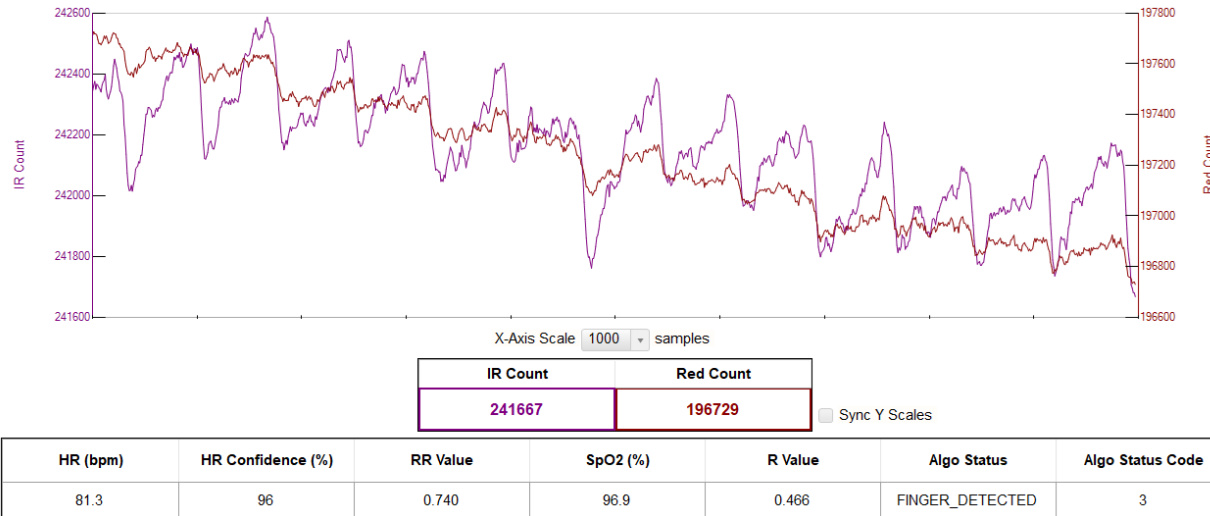


Custom design PCB for HR, ECG, SpO₂, Resp. Rate, Temp. & enviromental parameters measurement.

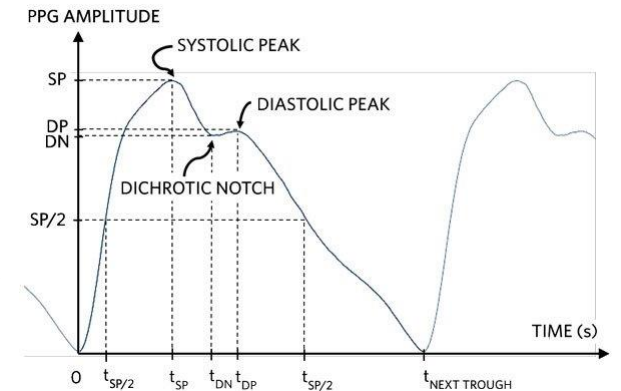
source: <https://www.analog.com/en/products/max32664.html>

Source: Original work by the author

Use case: PPG (SpO2, HR) AFE integration in a custom multichannel, multimodal system.



Raw PPG signals from AFE from convenient evaluation board (my finger on my desk 😊)



Source: Original work by the author



Drivers activity recognition



Natalia Piaseczna, MSc BEng,

Promoter: Dariusz Komorowski, Ph.D., D.Sc., BEng., Prof. of SUT,

Associate Promoter: Rafał Doniec, Ph.D., BEng.,

Department of Medical Informatics and Artificial Intelligence, Faculty of Biomedical Engineering,
Silesian University of Technology

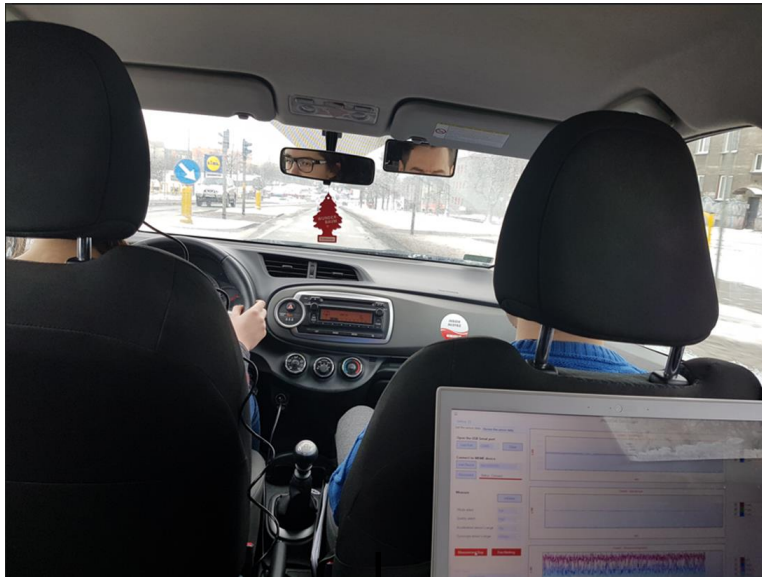
natalia.piaseczna@ieee.org

Aim of the study

1. Developing methodologies for analysis and classification and EOG data in the context of driving
2. Investigating the impact of vision impairment factors on driving safety
Development of methods for identifying the level of driver experience
3. Analysis of the differences between driving in real and simulated conditions
4. Development of methods for predicting car accidents
5. Creation of a database of data acquired under simulated conditions containing different types of activities of the person driving the vehicle.



Experimental setup



Real road conditions

car, laptop with dedicated software



Simulated conditions

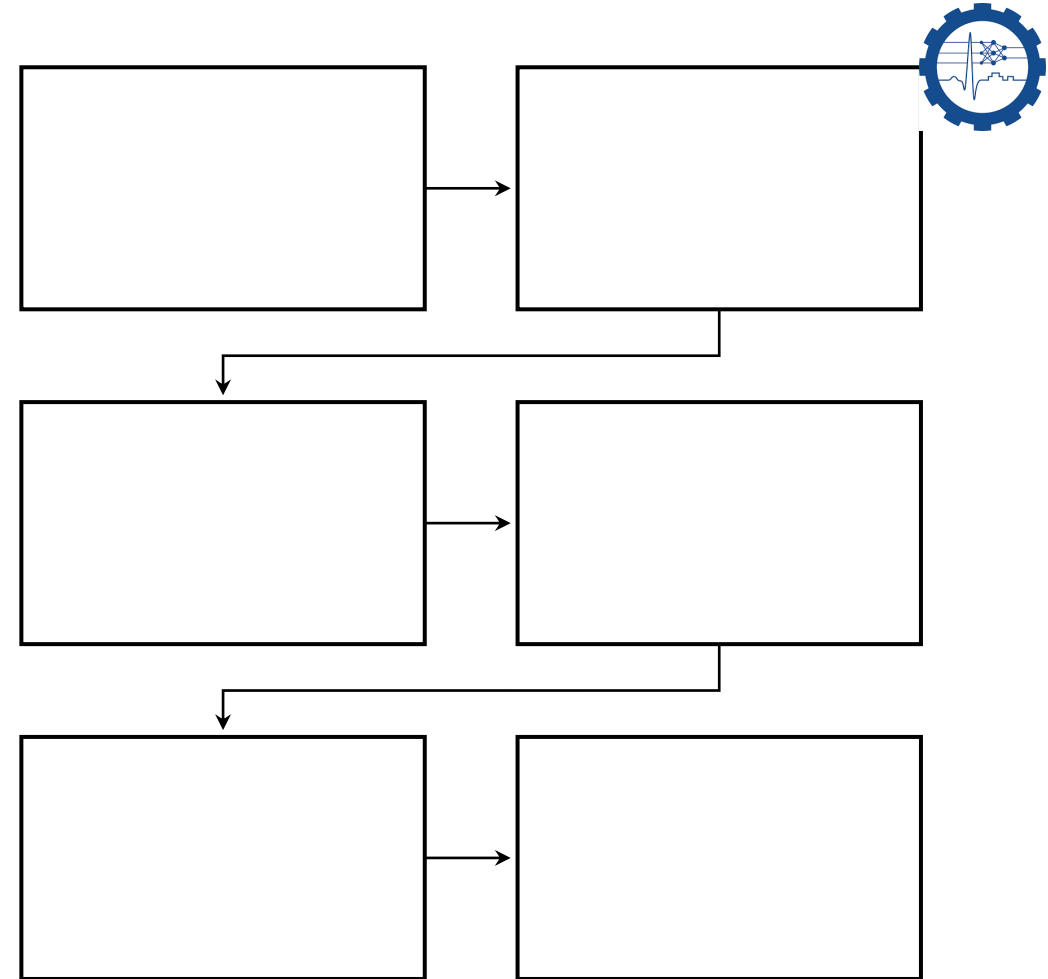
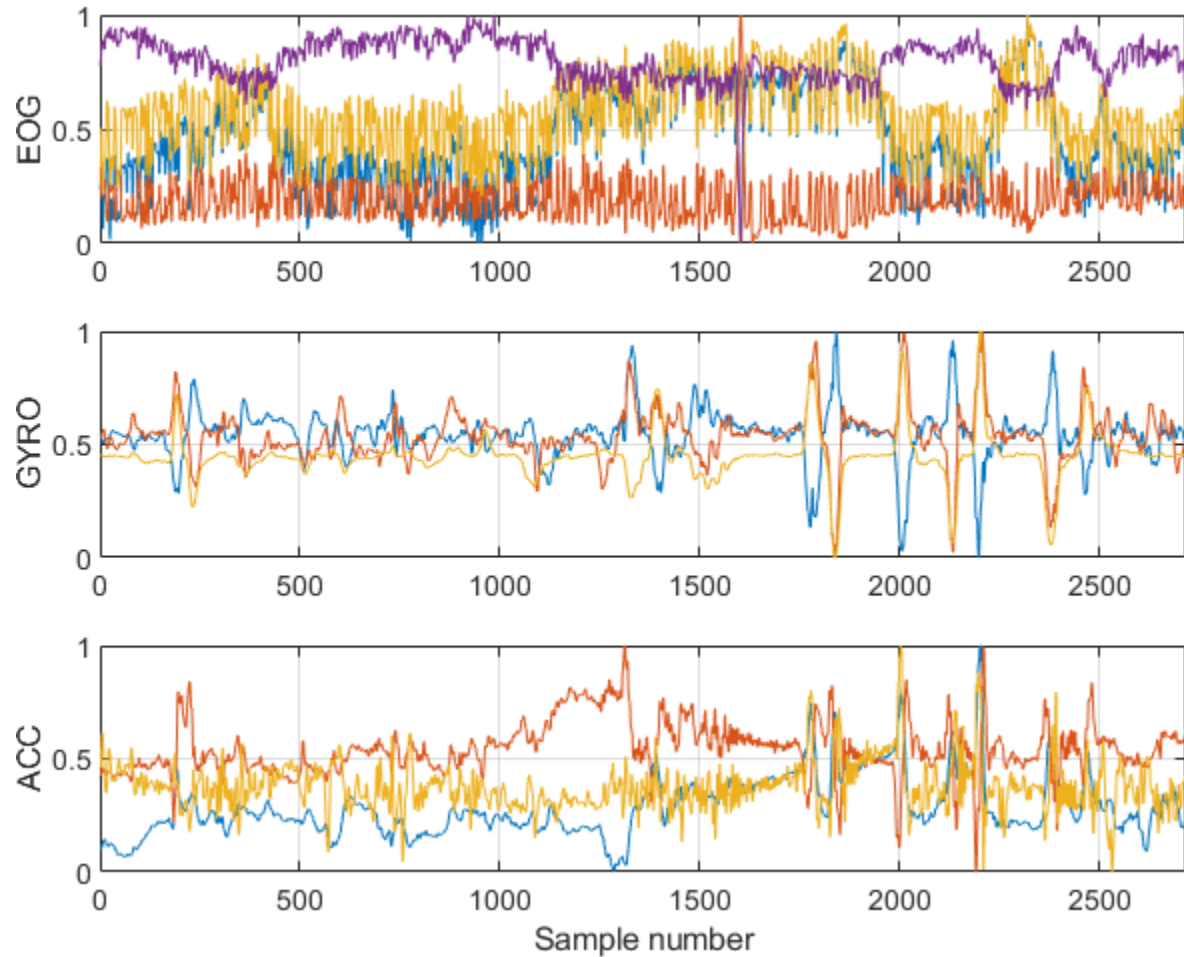
car simulator, laptop with dedicated software



Data acquisition

JINS MEME ES_R academic pack, 3-point EOG, 3-axes accelerometer and gyroscope

General methodology





Publications

1. Classification of recorded electrooculographic signals on drive activity for assessing four kind of driver inattention by bagged trees algorithm: a pilot study, DOI:10.1007/978-3-031-38430-1_18
2. The detection of alcohol intoxication using electrooculography signals from smart glasses and machine learning techniques, DOI:10.1016/j.sasc.2024.200078
3. Does glucose affect our vision? A preliminary study using smart glasses, DOI:10.1109/IEEECONF58974.2023.10404616
4. Sensor-based classification of primary and secondary car driver activities using convolutional neural networks, DOI:10.3390/s23125551
5. Classification of roads and types of public roads using EOG smart glasses and an algorithm based on machine learning while driving a car, DOI:10.3390/electronics11182960
6. The classifier algorithm for recognition of basic driving scenarios, DOI:10.1007/978-3-030-49666-1_28
7. Recognition of drivers' activity based on 1D convolutional neural network, DOI:10.3390/electronics9122002
8. Recognition of basic driving scenarios, ISBN 978-1-5386-1312-2

Analysis of heart rate variability based on electrocardiograms, seismocardiograms and gyrocardiograms

Szymon Sieciński, Ph.D., BEng.

Research assistant at the Institute of Medical Informatics, University of Lübeck, Germany
(Email: szymon.siecinski@uni-luebeck.de)

Lecturer at the Department of Clinical Engineering, Academy of Silesia, Katowice, Poland
(Email: szymon.siecinski@akademiaslaska.pl)

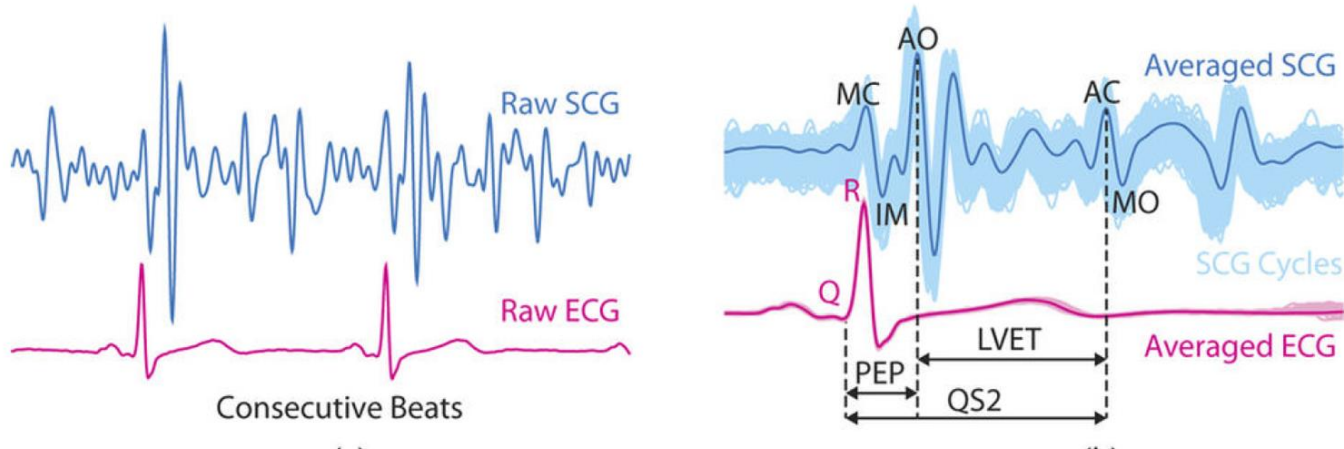
ORCID: 0000-0002-3801-3144

Promoter: Paweł Kostka, Ph.D., D.Sc., BEng., Prof. of SUT,



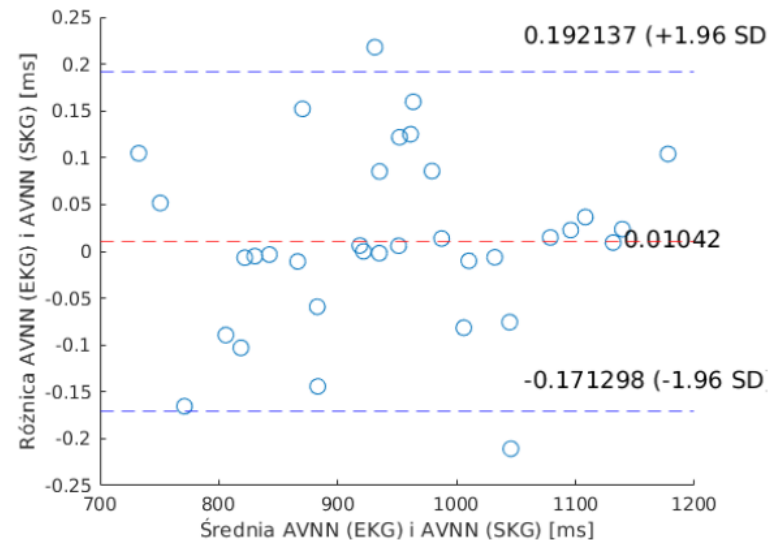
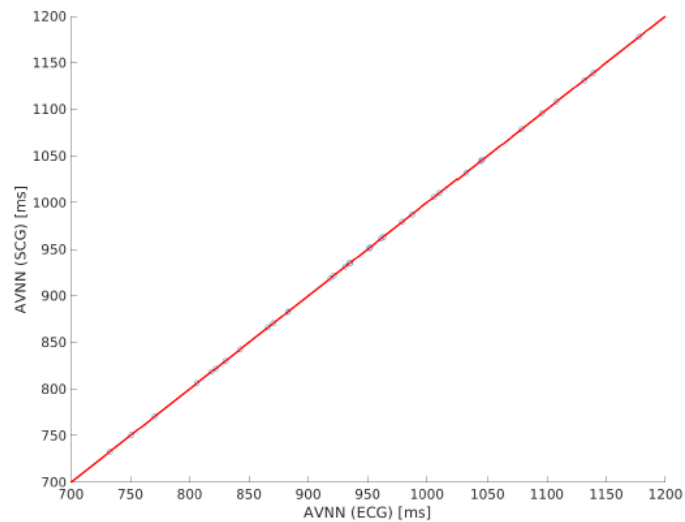
UNIVERSITÄT ZU LÜBECK
INSTITUTE OF MEDICAL INFORMATICS

Seismocardiogram (SCG) example:



Analysis steps:

- Detection of heartbeats in ECG & SCG signals;
- Calculation of heartbeat intervals (NN) for each signal analyzed;
- Perform HRV analysis separately for each signal:
 - Temporal analysis (AVNN, SDNN, RMSSD, pNN50),
 - Frequency analysis (TP, LF, VLF, HF, LF/HF),
 - Nonlinear analysis (SD1, SD2, SD1/SD2, EA, VAI, VLI)



AVNN compliance analysis for ECG and SCG: a) correlation, b) Bland-Altman graph

OPEN

Surface Chest Motion Decomposition for Cardiovascular Monitoring

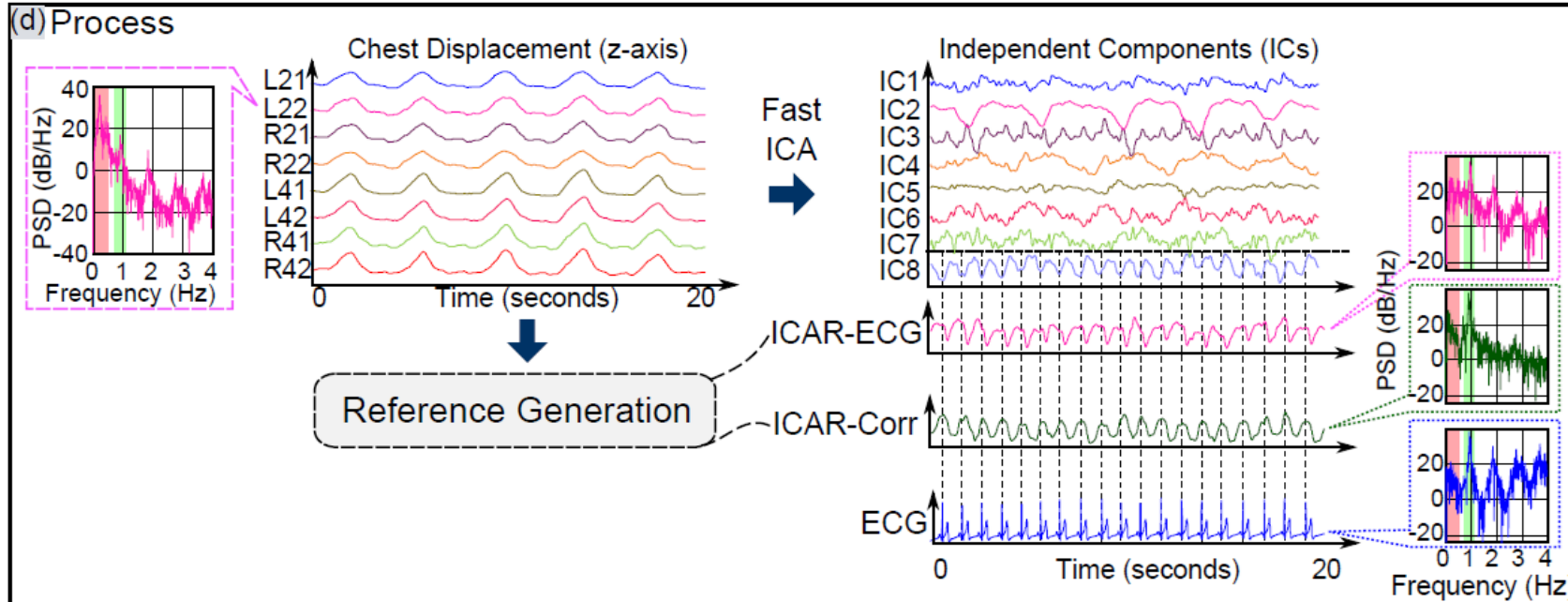
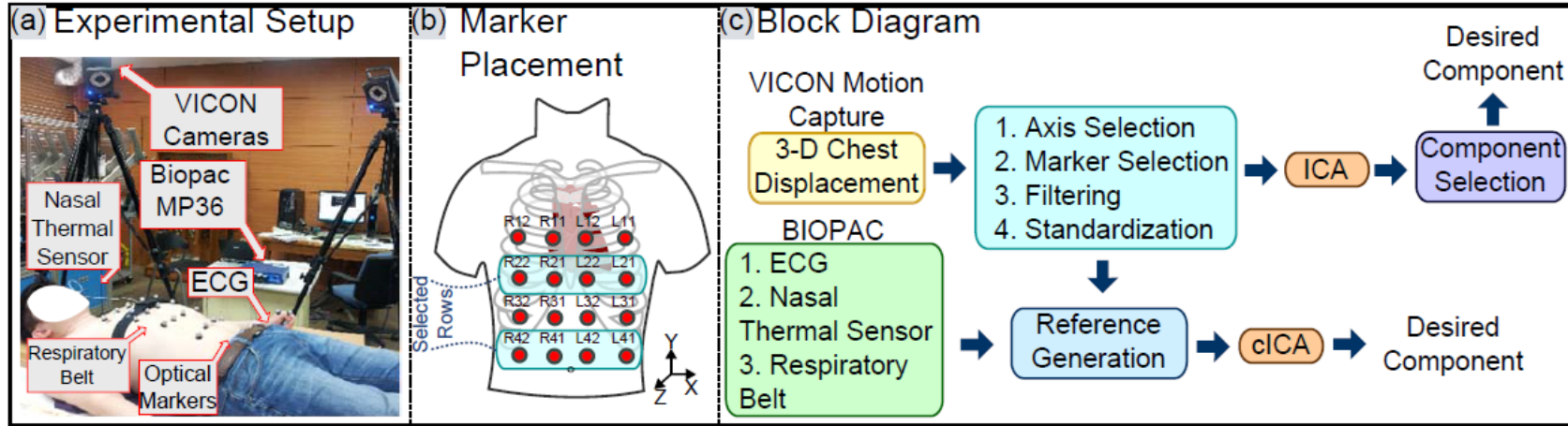
SUBJECT AREAS:

MEDICAL IMAGING

BIOMEDICAL ENGINEERING

Ghufran Shafiq & Kalyana C. Veluvolu

School of Electronics Engineering, College of IT Engineering, Kyungpook National University, Daegu, South Korea 702-701.



Biomedical signal acquisition and processing methods for “wearable” systems

Marek Czerw MSc, Eng.

Implementation PhD

Promoter: Paweł Kostka, Ph.D., D.Sc., BEng., Prof. of SUT,

Associate Promoter: Janusz Wróbel, Ph.D., D.Sc., BEng.,

Łukasiewicz Research Network – Krakow Institute of Technology,
Center for Biomedical Engineering Zabrze, SUT.

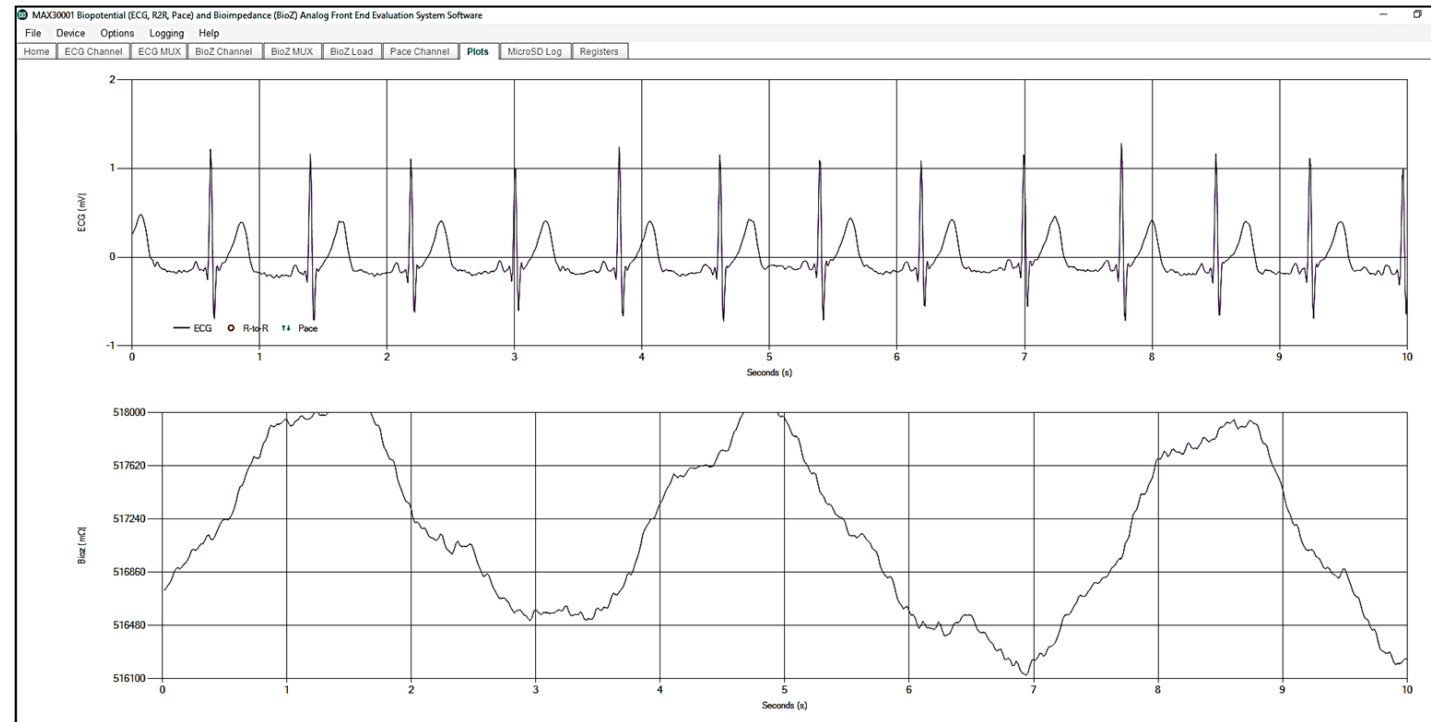
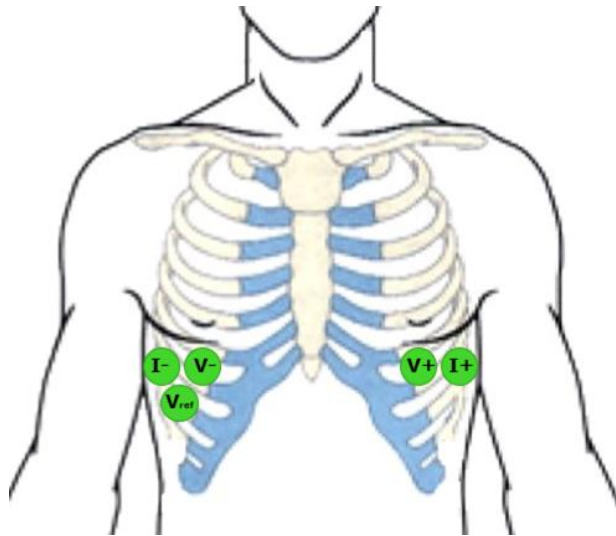
marek.czerw@kit.lukasiewicz.gov.pl

janusz.wrobel@kit.lukasiewicz.gov.pl



Development of measurement methods for biomedical parameters (including HRV & Respiratory curve → Respiratory Rate RR[brpm]+other resp. params.)

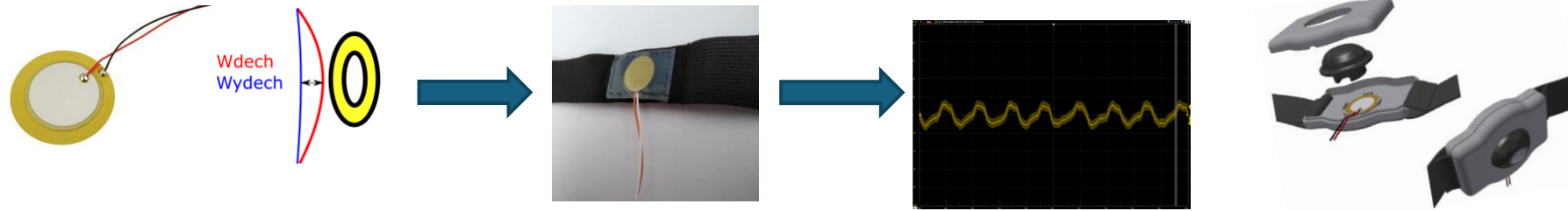
Integrated measuring transducer for ECG and bioimpedance recording



The **impedance Z** is measured by introducing an alternating electric **current** of $F=50\text{kHz}$, and $I_{RMS}=1\text{mA}$ through two electrodes, and **measuring the voltage** with the receiving electrodes, an **ECG** is also recorded from the same electrodes

Comparison of methods for measuring respiratory parameters

Piezoelectric method



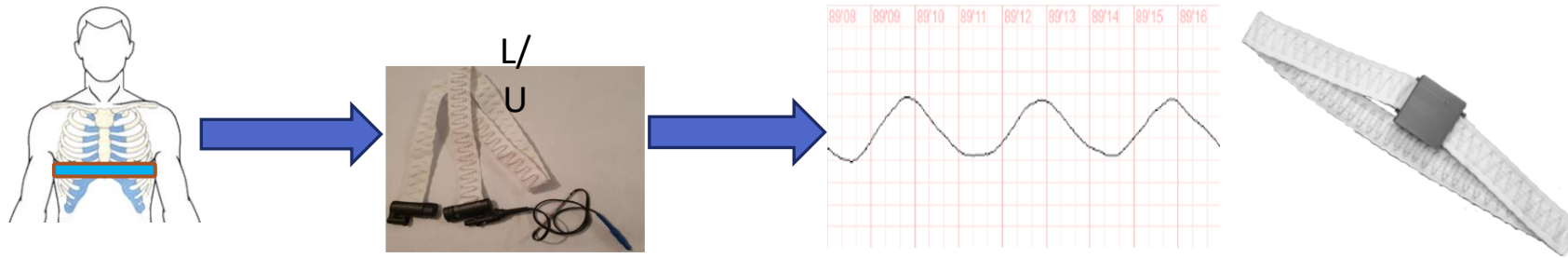
The movement of the chest caused by inhalation and exhalation causes a change in pressure on the piezo diaphragm, which in turn produces tension proportional to the movement of the chest

Resistance method



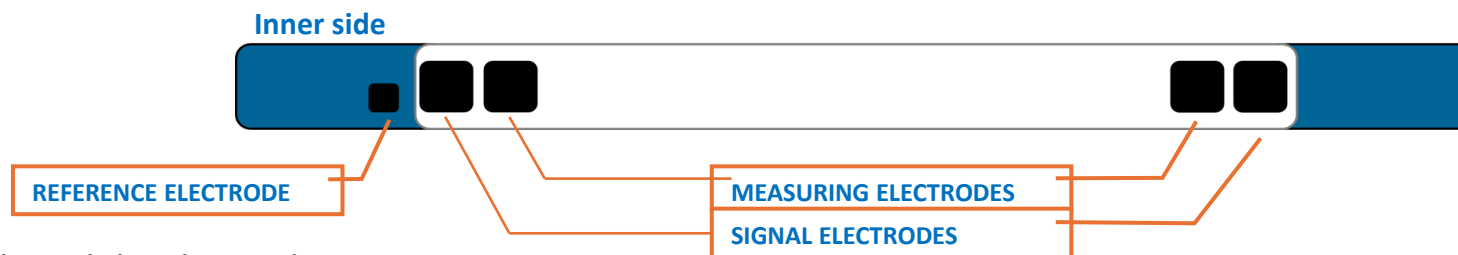
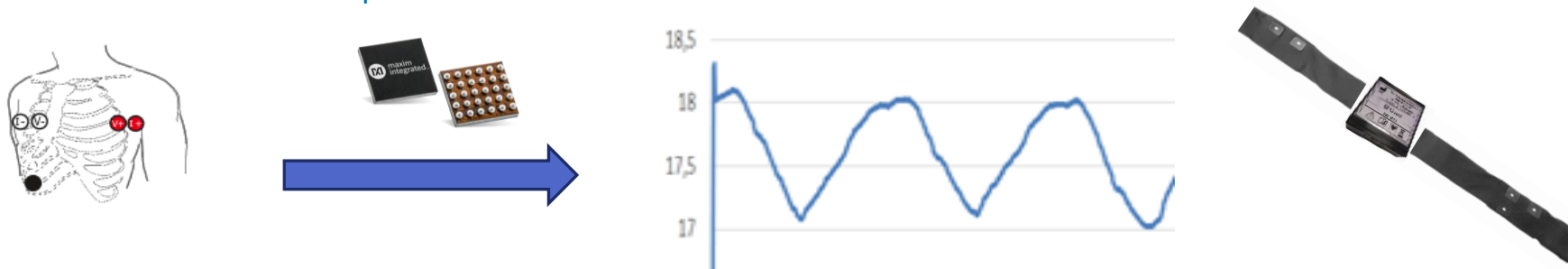
A method of monitoring breathing using a conductive tape that changes its resistance when stretched

Induction method: involves converting changes in inductance into PWM pulse width and then into a change in voltage.

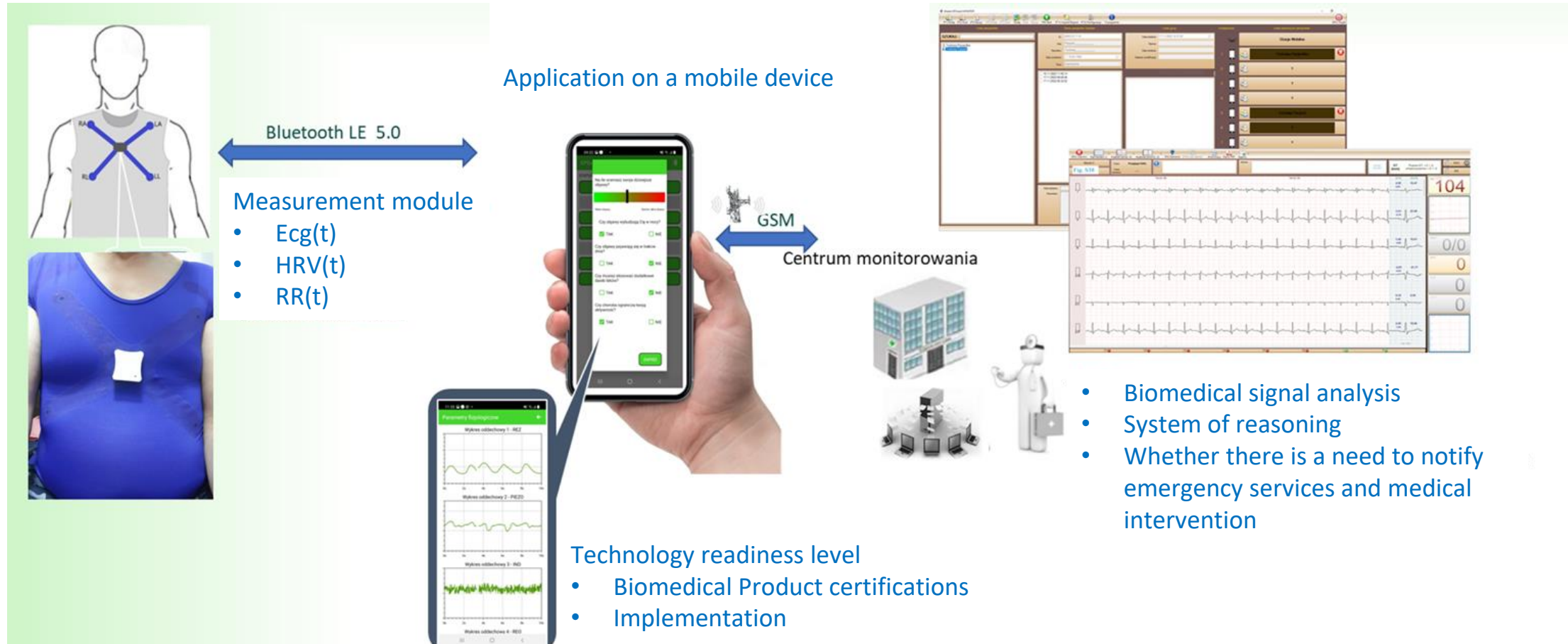


Rheographic method: involves recording changes in chest impedance during breathing using a dedicated integrated transducer.

During inspiration, there is an increase in the volume of gas in the chest which decreases the conductivity and the area of the chest increases and with it the measured impedance .



Structure of a final wearable system for biomedical signal acquisition and processing



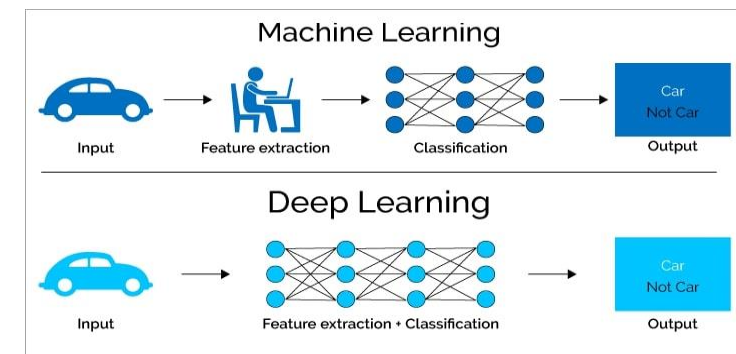
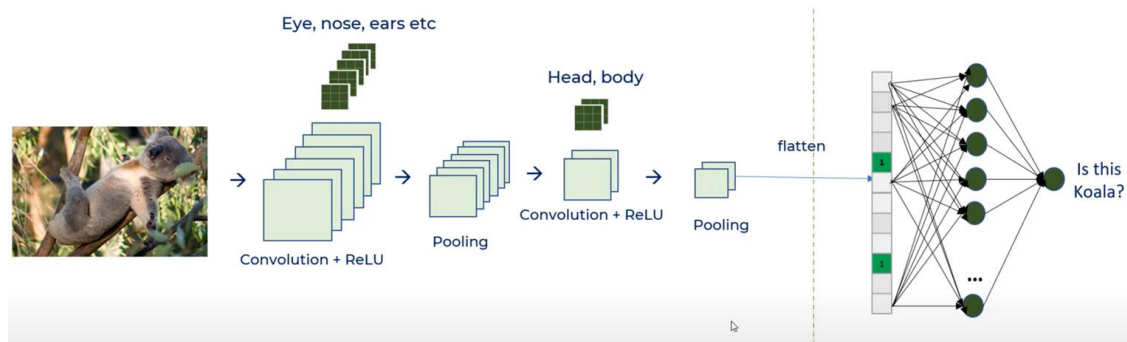


Conclusions

- DSP and feature extraction (FE) - probably **still relevant** in specialized tasks, especially e.g. for processing 1-dimensional, multimodal signals;

- Deep Learning methods (without an explicit FE stage) in processing:

- Images,
- Movies,
- Audio
- Text,



- Deep learning AI with CNN networks is, of course, already working effectively in the role of 'creative' - generative

VIBE Project

Virtual biomedical engineering and stem/steam education

Basic information

Project ID: VIBE

Project start date: 1 November 2021

Project end date: 31 October 2024

Coordinator: University of Pécs, Pécs, Hungary

Partners

Universidade do Porto, Porto, Portugal

DEX Innovation Centre, Liberec, Czech Republic

Silesian Univ. of Technology, BE faculty, Poland.

<https://vibe-project.pte.hu/>

Project outcomes

- Spreading and widening the knowledge and awareness of VR/AR-based learning
- Higher number of students interested in STEM/STEAM or medical fields and increased level of diversity
- More immersive and overall improved VR environment
- A completely new curriculum (Biomedical Engineering BSc) developed using the VR platform as a co-creation and collaboration tool.
- Maintaining the international cooperation network established in the project beyond the scope of EU funding.

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I would like to thank our partners very much for:

- *cooperation,* ✓
- *support,* ✓
- *motivation* ✓

<https://vibe-project.pte.hu/>

